

# Applying Constraints to the Electrocardiographic Inverse Problem

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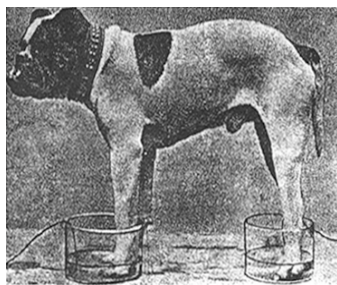
•Cardiovascular Research and  
Training Institute (CVRTI)

•Northeastern University, CDSP,  
ECE Department



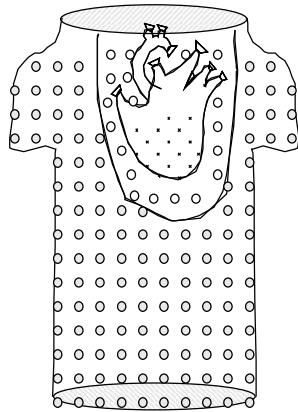
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## Electrocardiography



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# Electrocardiographic Mapping

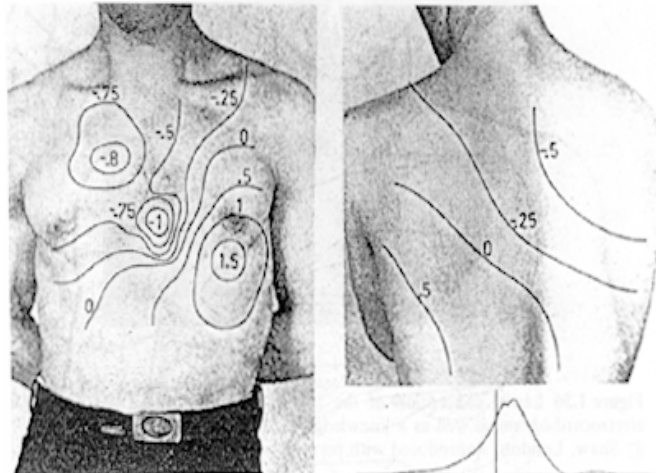


- Bioelectric Potentials
- Goals
  - Higher spatial density
  - Imaging modality
- Measurements
  - Body surface
  - Heart surfaces
  - Heart volume



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# Body Surface Potential Mapping

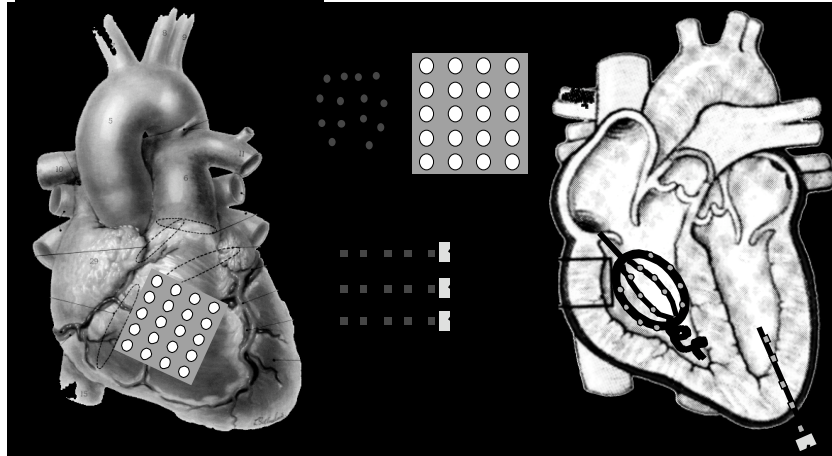


Taccardi  
et al,  
Circ.,  
1963



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# Cardiac Mapping

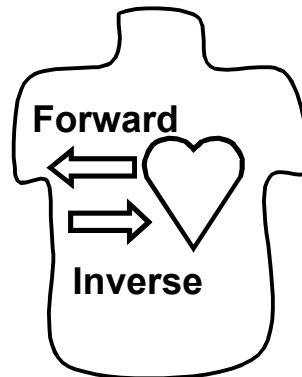
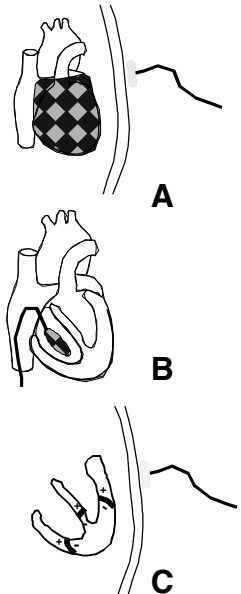


- Sampling Density
- Surface or volume



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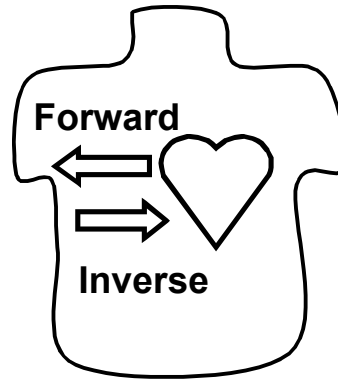
# Inverse Problems in Electrocardiography



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# Epicardial Inverse Problem

- **Definition**
  - Estimate sources from remote measurements
- **Motivation**
  - Noninvasive detection of abnormalities
  - Spatial smoothing and attenuation



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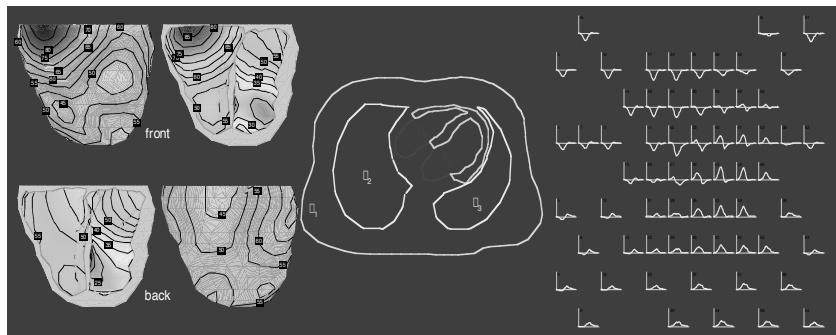
# Forward/Inverse Problem

Forward problem

Epicardial/Endocardial  
Activation Time

Geometric  
Model

Body Surface  
Potentials



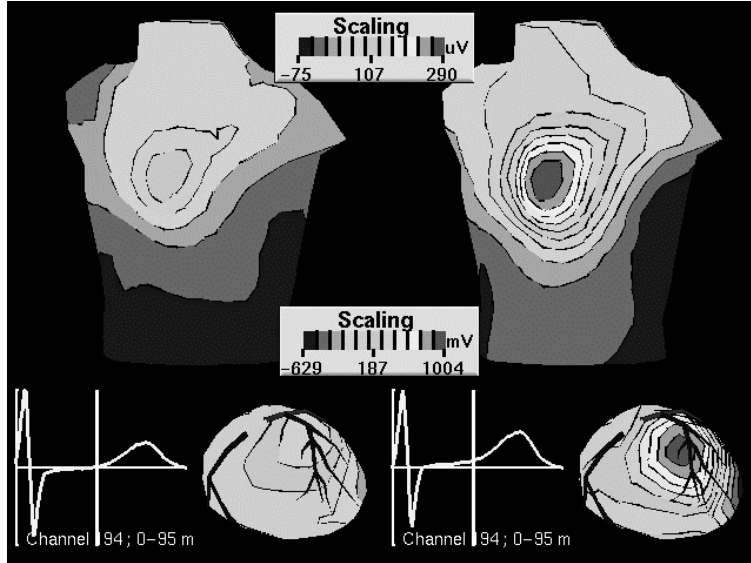
Inverse problem

Thom Oostendorp,  
Univ. of Nijmegen

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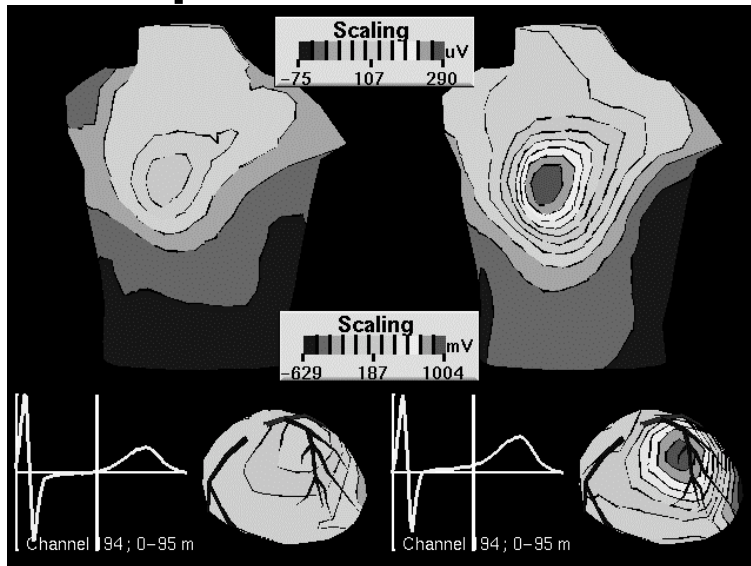


# Sample Problem: PTCA



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# Sample Problem: PTCA



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## Elements of the Inverse Problem

- **Components**
  - Source description
  - Geometry/conductivity
  - Forward solution
  - “Inversion” method (regularization)
- **Challenges**
  - Inverse is ill-posed
  - Solution ill-conditioned



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## Inverse Problem Research

- **Role of geometry/conductivity**
- **Numerical methods**
- **Improving accuracy to clinical levels**
- **Regularization**
  - *A priori* constraints versus fidelity to measurements



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# Regularization

- **Current questions**
  - Choice of constraints/weights
  - Effects of errors
  - Reliability
- **Contemporary approaches**
  - Multiple Constraints
  - Time Varying Constraints
  - Tuned constraints
  - Multisource constraints



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# Tikhonov Approach

Problem formulation

$$\mathbf{y}(k) = \mathbf{A} \cdot \mathbf{h}(k) + \mathbf{e}(k) \quad k = 1, 2, \dots, L$$

Constraint

$$\hat{\mathbf{h}}_{\lambda} = \arg \min_{\mathbf{x}} \left( \|\mathbf{y} - \mathbf{A}\mathbf{x}\|^2 + \lambda^2 \|\mathbf{R}\mathbf{x}\|^2 \right),$$

Solution

$$\hat{\mathbf{h}}_{\lambda} = (\mathbf{A}^T \mathbf{A} + \lambda^2 \mathbf{R}^T \mathbf{R})^{-1} \mathbf{A}^T \mathbf{y}$$



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## Multiple Constraints

For k constraints

$$\hat{\mathbf{h}}_{\lambda} = \arg \min_{\mathbf{x}} \left( \|\mathbf{y} - \mathbf{A}\mathbf{x}\|^2 + \sum_{i=1}^k \lambda_i^2 \|\mathbf{R}_i \mathbf{x}\|^2 \right)$$

with solution

$$\hat{\mathbf{h}}_{\lambda} = [\mathbf{A}^T \mathbf{A} + \sum_{i=1}^k \lambda_i^2 \mathbf{R}_i^T \mathbf{R}_i]^{-1} \mathbf{A}^T \mathbf{y}.$$



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## Dual Spatial Constraints

For two spatial constraints:

$$\hat{\mathbf{h}}_{\lambda} = (\mathbf{A}^T \mathbf{A} + \lambda_1^2 \mathbf{R}_1^T \mathbf{R}_1 + \lambda_2^2 \mathbf{R}_2^T \mathbf{R}_2)^{-1} \mathbf{A}^T \mathbf{y}.$$

Note: two regularization factors required



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## Joint Time-Space Constraints

Redefine  $\mathbf{y}$ ,  $\mathbf{h}$ ,  $\mathbf{A}$ :

$$\bar{\mathbf{y}} = \bar{\mathbf{A}}\mathbf{h} + \bar{\mathbf{e}}$$

$$\bar{\mathbf{A}} = \begin{pmatrix} \mathbf{A} & \mathbf{0} & \mathbf{0} & \dots & \mathbf{0} \\ \mathbf{0} & \mathbf{A} & \mathbf{0} & \dots & \mathbf{0} \\ \mathbf{0} & \mathbf{0} & \mathbf{A} & \dots & \mathbf{0} \\ & & & \dots & \\ \mathbf{0} & \mathbf{0} & \mathbf{0} & \dots & \mathbf{A} \end{pmatrix}.$$

And write a new minimization equation:

$$\hat{\mathbf{h}} = \arg \min_{\bar{\mathbf{x}}} \left( \|\bar{\mathbf{A}}\bar{\mathbf{x}} - \bar{\mathbf{y}}\|^2 + \sum_{i=1}^{k_s} \lambda_i^2 \|\bar{\mathbf{R}}_i \bar{\mathbf{x}}\|^2 + \sum_{i=1}^{k_t} \eta_i^2 \|\bar{\mathbf{T}}_i \bar{\mathbf{x}}\|^2 \right).$$



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## Joint Time-Space Constraints

General solution:

$$\hat{\mathbf{h}} = (\bar{\mathbf{A}}^T \bar{\mathbf{A}} + \sum_{i=1}^{k_s} \lambda_i^2 \bar{\mathbf{R}}_i^T \bar{\mathbf{R}}_i + \sum_{i=1}^{k_t} \eta_i^2 \bar{\mathbf{T}}_i^T \bar{\mathbf{T}}_i)^{-1} \bar{\mathbf{A}}^T \bar{\mathbf{y}}$$

For a single space and time constraint:

$$\begin{aligned} \hat{\mathbf{h}} &= (\bar{\mathbf{A}}^T \bar{\mathbf{A}} + \lambda^2 \bar{\mathbf{R}}^T \bar{\mathbf{R}} + \eta^2 \bar{\mathbf{T}}^T \bar{\mathbf{T}})^{-1} \bar{\mathbf{A}}^T \bar{\mathbf{y}} \\ &= [\mathbf{I}_L \otimes (\mathbf{A}^T \mathbf{A}) + \lambda^2 \mathbf{I}_L \otimes \mathbf{R}^T \mathbf{R} + \eta^2 (\mathbf{T}^T \mathbf{T}) \otimes \mathbf{I}_N]^{-1} \cdot (\mathbf{I}_L \otimes \mathbf{A}^T) \bar{\mathbf{y}}. \end{aligned}$$

Note: two regularization factors and implicit temporal factor



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## Determining Weights

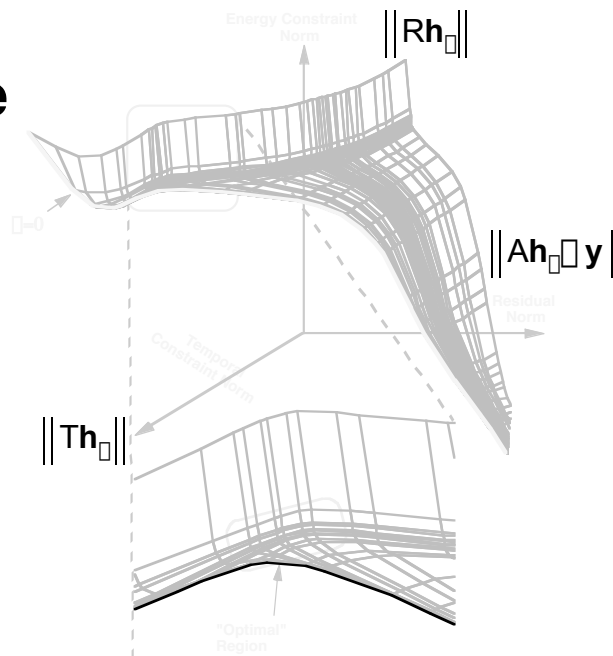
- Based on *a posteriori* information
- *Ad hoc* schemes
  - CRESO: composite residual and smooth operator
  - BNC: bounded norm constraint
  - AIC: Akaike information criterion
  - L-curve: residual norm vs. solution seminorm



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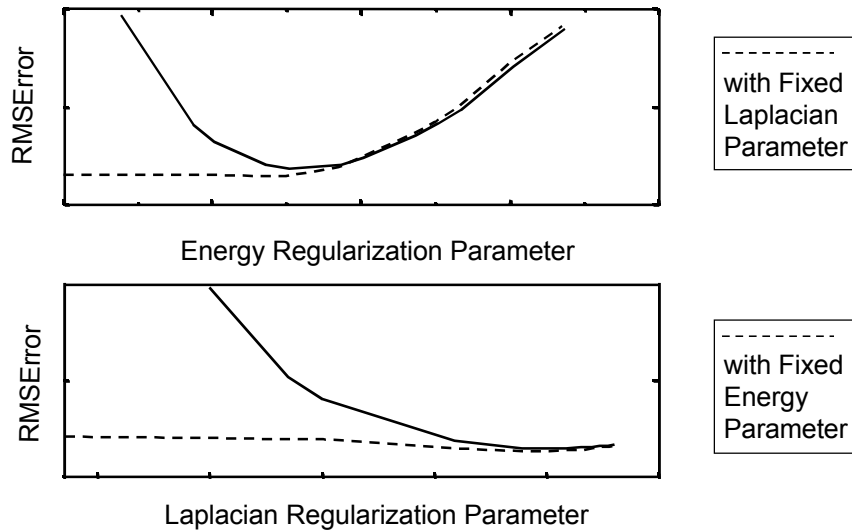
## L-Surface

- Natural extension of single constraint approach
- “Knee” point becomes a region



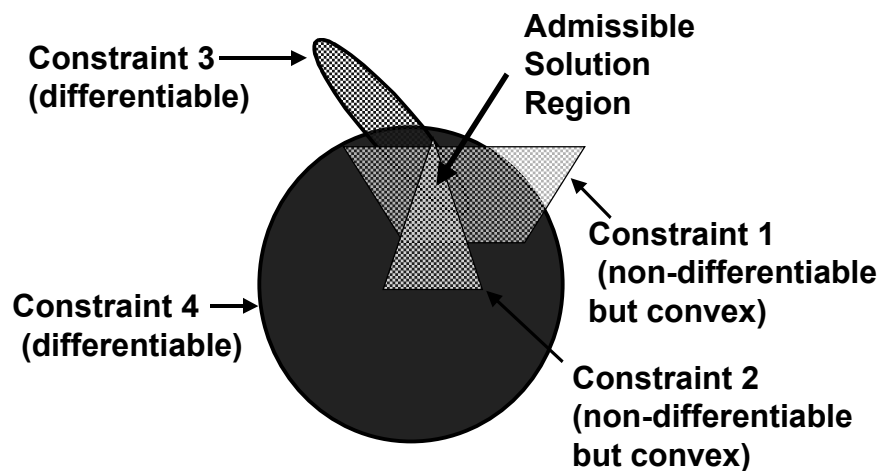
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# Joint Regularization Results



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# Admissible Solution Approach



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## Single Constraint

Define  $\phi(\mathbf{x})$  s.t.

$$\phi(\mathbf{x}) : \mathcal{R}^N \rightarrow \mathcal{R}$$

with the constraint such that

$$\phi(\mathbf{x}) - \epsilon < 0.$$

that satisfies the convex condition

$$\phi(\alpha\mathbf{x} + (1 - \alpha)\mathbf{y}) \leq \alpha\phi(\mathbf{x}) + (1 - \alpha)\phi(\mathbf{y}) \quad \forall \alpha \in [0, 1].$$



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## Multiple Constraints

Define multiple constraints  $\phi_i(\mathbf{x})$

$$(\phi_i(\mathbf{x}) - \epsilon_i) \in \mathcal{H}, \text{ for } i = 1, 2, \dots, m.$$

so that the set of these

$$\{\mathbf{x} : \phi(\mathbf{x}) < 0\}$$

represents the intersection of all constraints. When they satisfy the joint condition

$$\phi(\mathbf{x}) \leq 0$$

Then the resulting  $\mathbf{x}$  is the *admissible solution*



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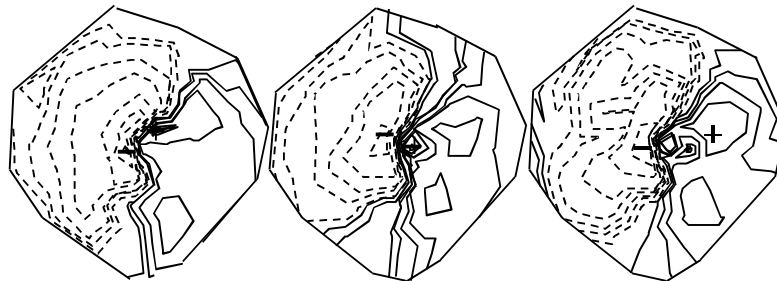
## Examples of Constraints

- Residual constraint  $\phi(\mathbf{x}) = \|\mathbf{Ax} - \mathbf{y}\|_2^2$
- Regularization constraints  $\phi(\mathbf{x}) = \|\mathbf{Rx}\|_2^2$
- Tikhonov constraints  $\phi_\lambda(\mathbf{x}) = \left\| \begin{pmatrix} \mathbf{A} \\ \sqrt{\lambda}\mathbf{R} \end{pmatrix} \mathbf{x} - \begin{pmatrix} \mathbf{b} \\ \mathbf{0} \end{pmatrix} \right\|_2^2$
- Spatiotemporal constraints
- Weighted constraints
- Novel constraints



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## Admissible Solution Results



Original

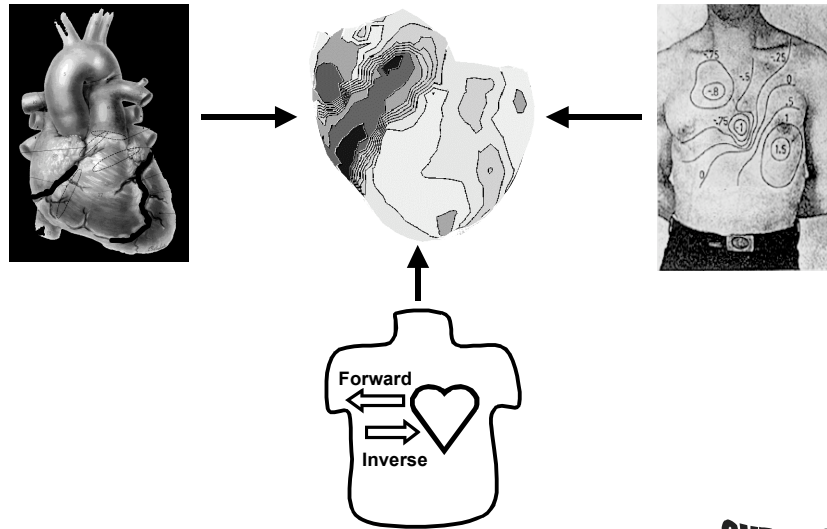
Regularized

Admissible  
Solution



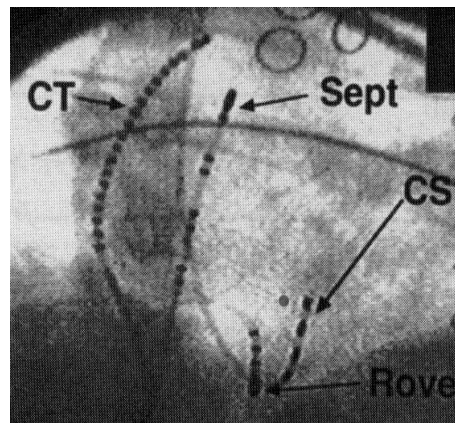
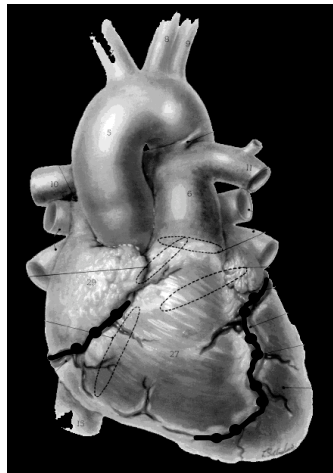
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## Combining Information Sources



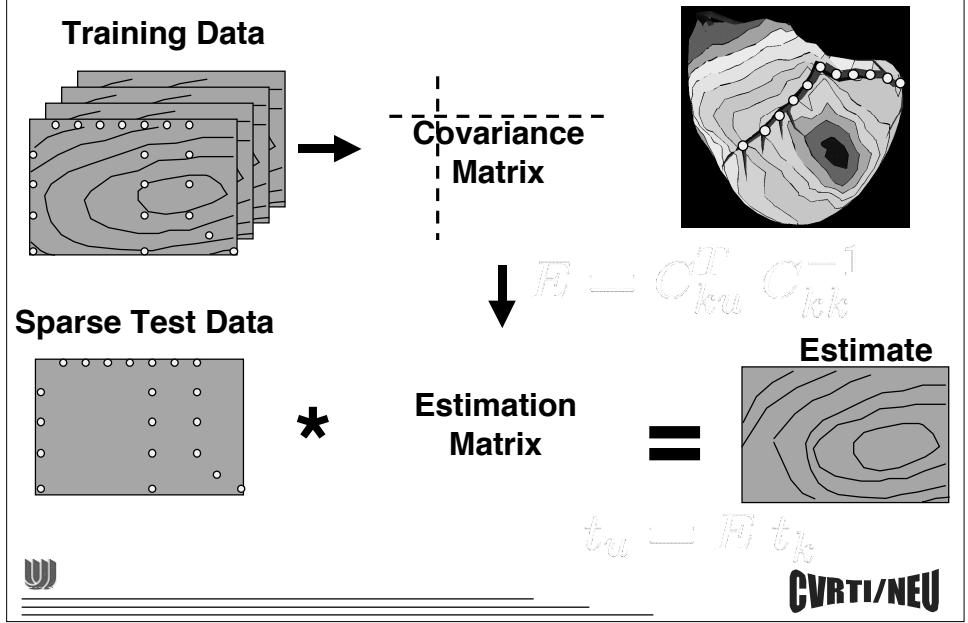
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## Venous Catheter Based Mapping

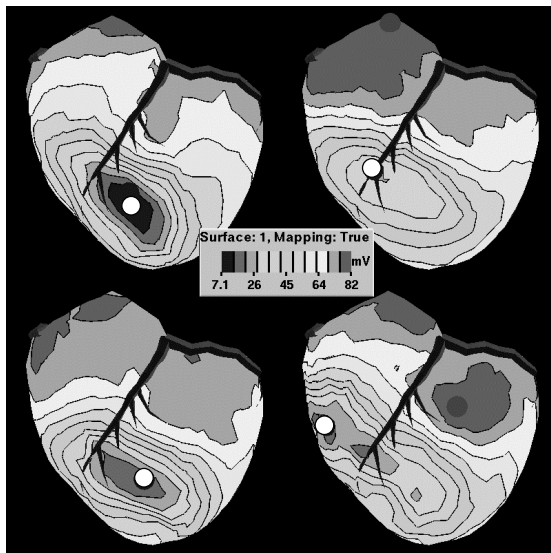


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# Statistical Estimation



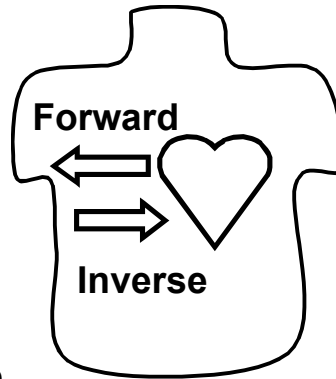
# Estimated Activation Maps



- Training set composition
- Lead selection

# Augmented Inverse Problem

Torso geometry  
+  
Body-Surface Potentials  
+  
Sparse Epicardial Potentials  
+  
Inverse Solution



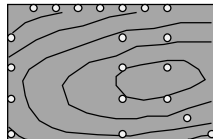
Epicardial Map



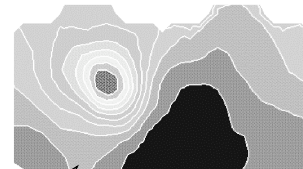
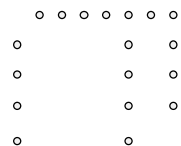
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# Subtraction Approach

*Unknown*

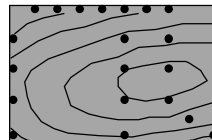


*Known*



- 1) Subtract known epicardial potentials
- 2) Solve reduced inverse problem

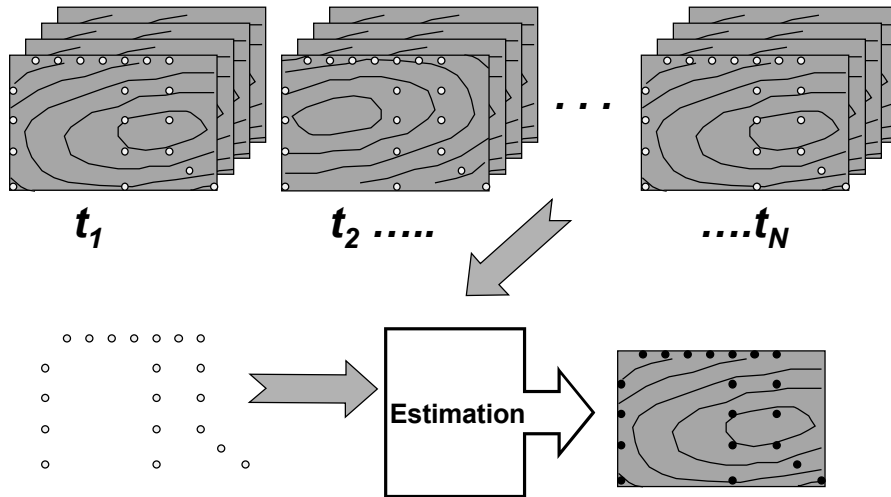
Inverse  
(Tikhonov)



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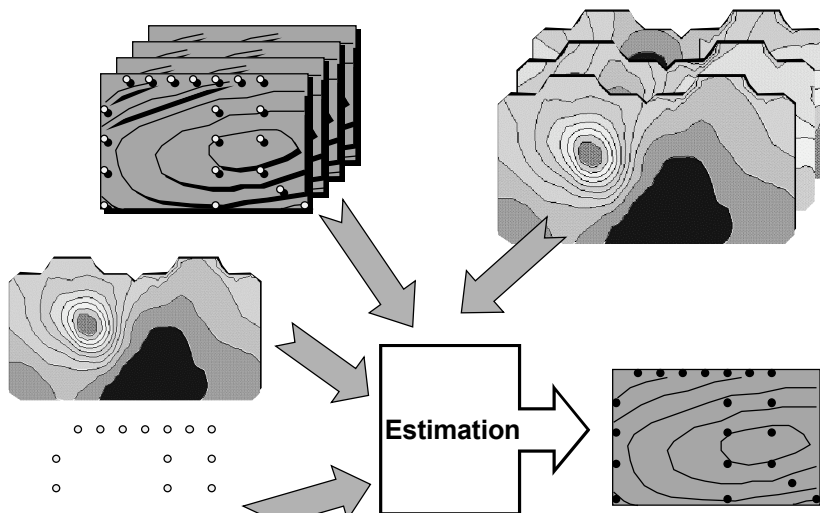


# Epicardial Estimation



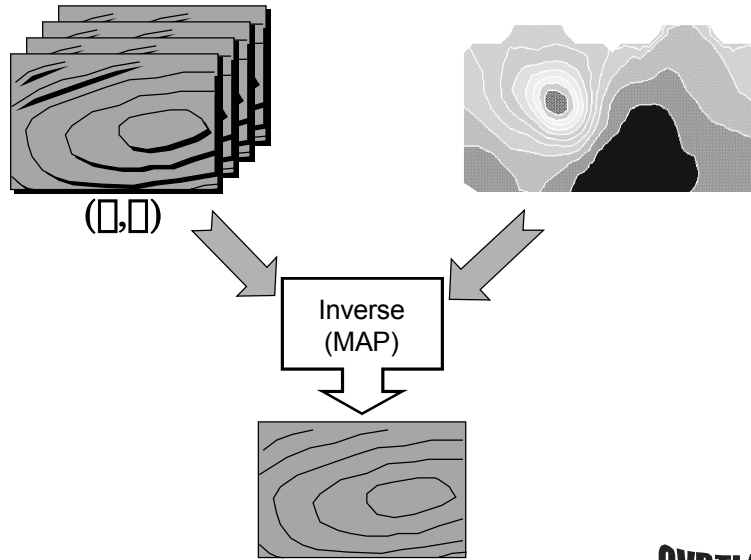
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# Combined Estimation



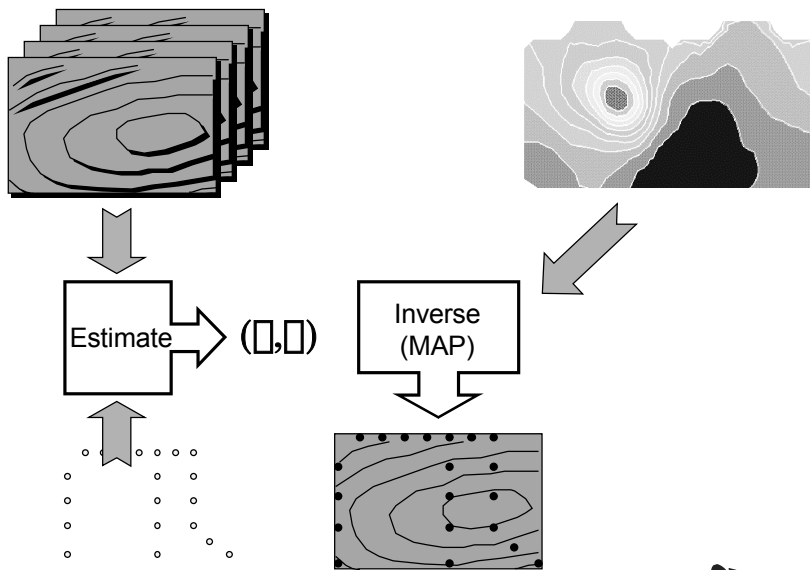
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# Bayesian Approach



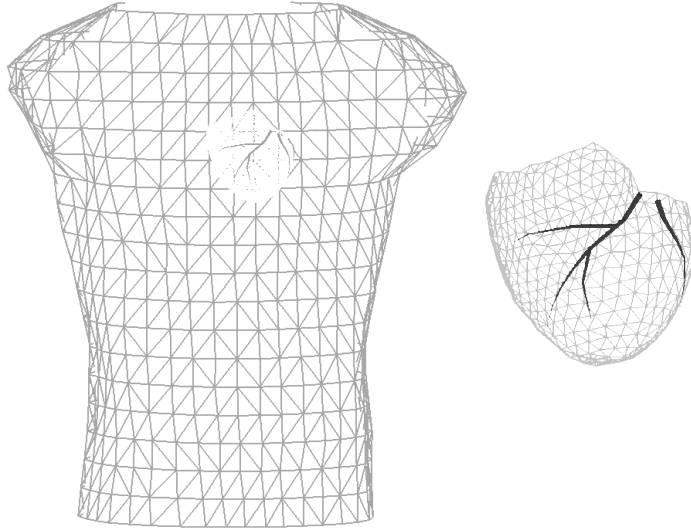
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# Hybrid Approach



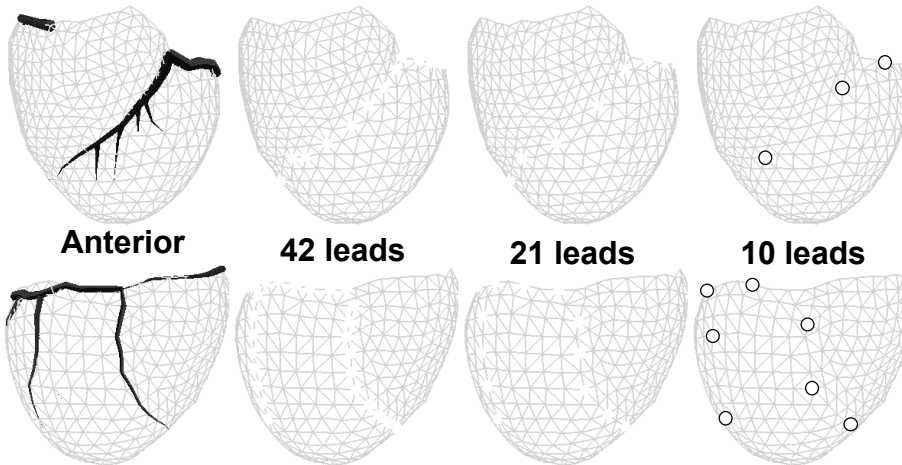
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# Tank/Heart Geometry



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# Test Lead Sets



**Anterior**

**42 leads**

**21 leads**

**10 leads**

**Posterior**



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## Simulation Study

- 490 lead measured sock data
- Surrogate catheter potentials
  - 42 sites
  - + Gaussian noise
- Torso potentials
  - Calculated noise-free using forward model
  - + Gaussian noise



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## Leave-One-Experiment Out Protocol

### Training Data

LV Paced  
Beats



Mixed  
Paced  
Beats

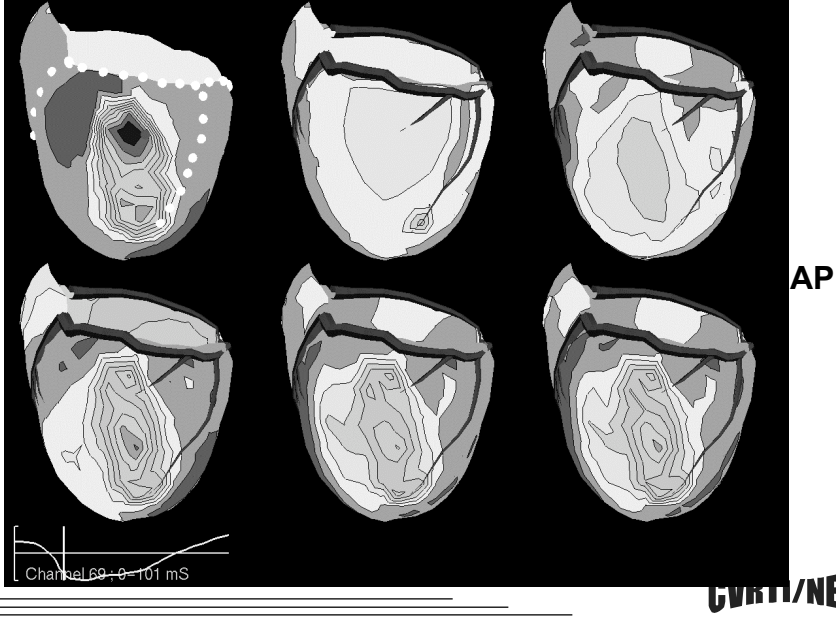


### Test Data

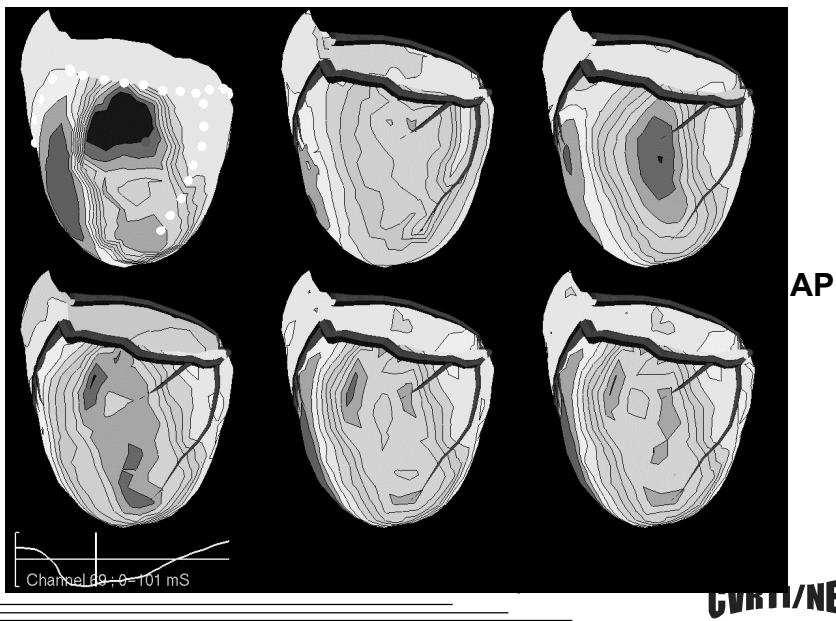


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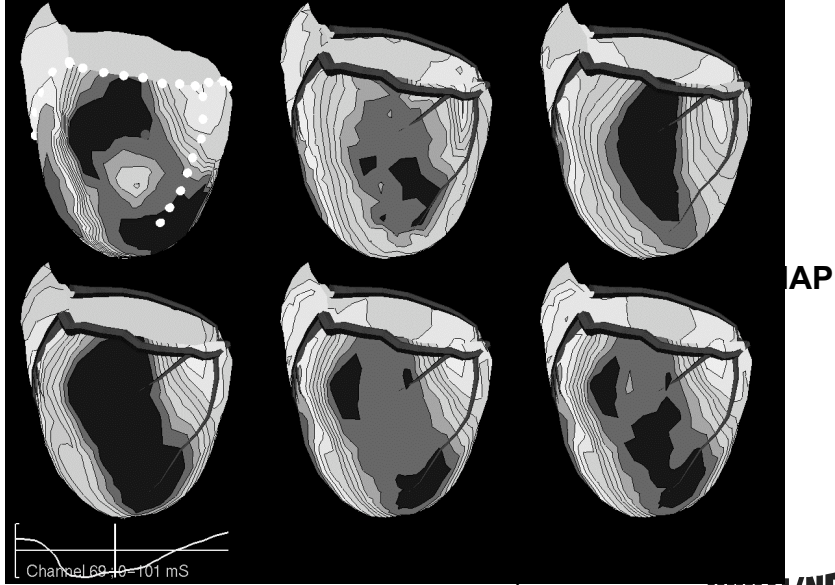
## LV Pacing (LV-23 ms)



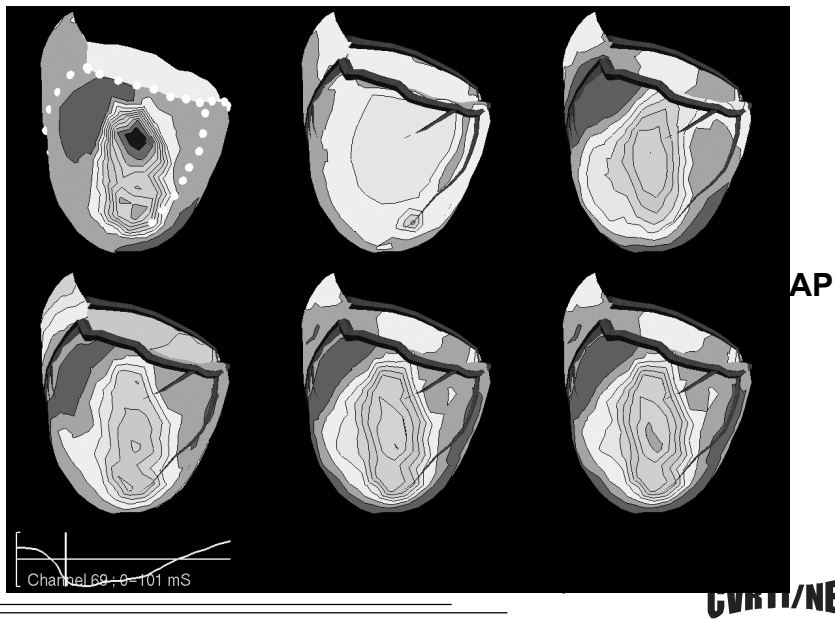
## LV Pacing (LV-38 ms)



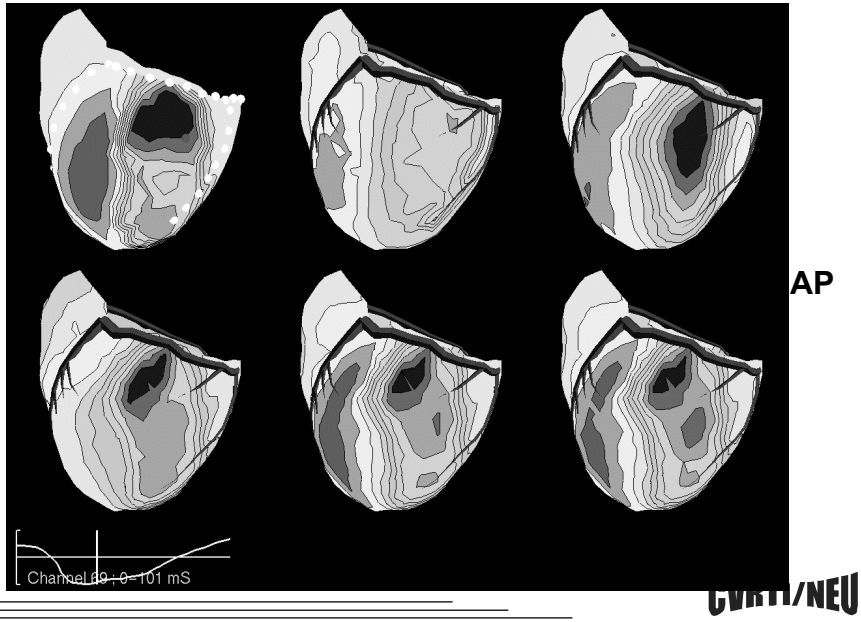
## LV Pacing (LV-47 ms)



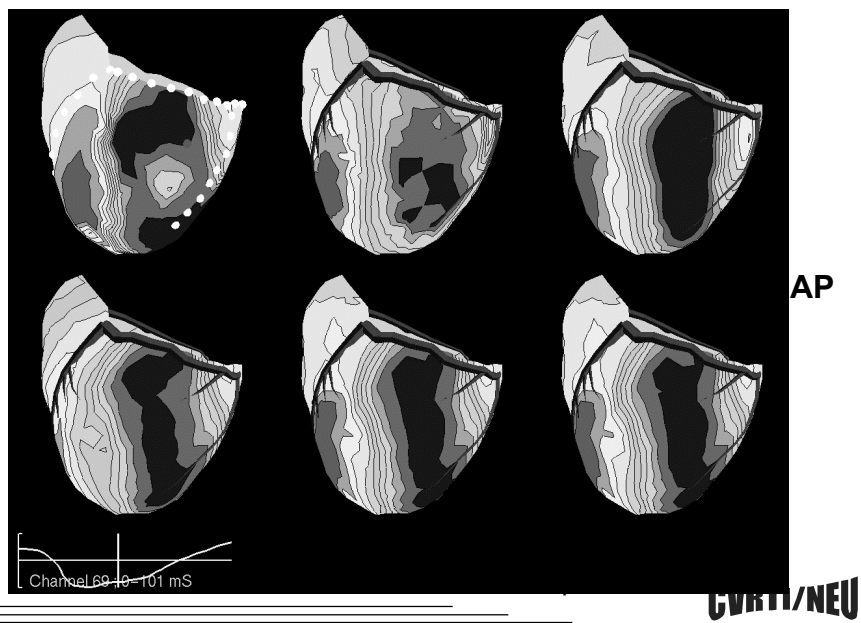
## LV Pacing (Mixed-23 ms)



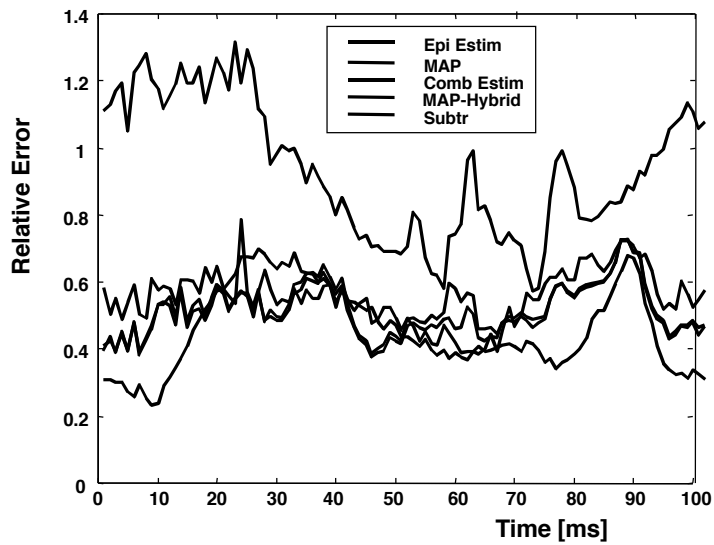
## LV Pacing (Mixed-38 ms)



## LV Pacing (Mixed-47 ms)

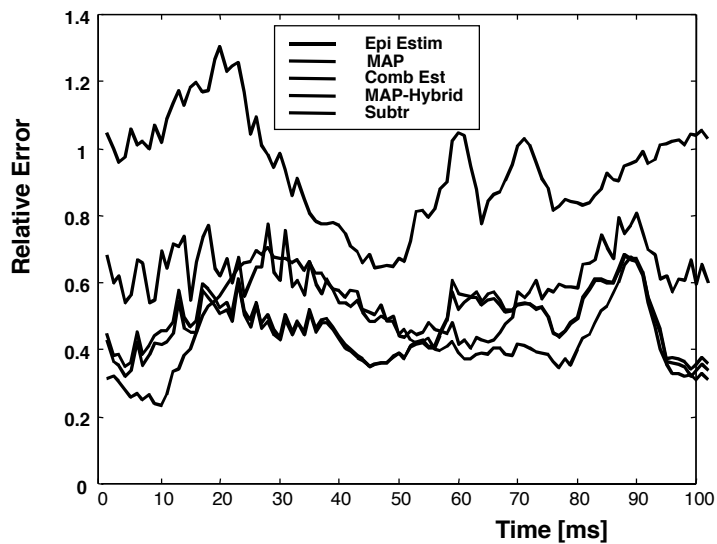


## Relative Error (31-LV)



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## Relative Error (31-Mixed)



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## Estimation Findings

- **Estimation alone: noisy, unstable results**
- **Estimation + inverse: smoothing improves stability**



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## Inverse Solution Findings

- **All solutions better than simple Tikhonov**
- **MAP usually improved with addition of catheter measurements (Hybrid MAP)**



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## Role of Statistics (Training)

- Generally helps
- But can add artifacts, e.g., spurious breakthroughs or wavefronts
- Torso potentials can reduce artifacts



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## Acknowledgements

- CVRTI
    - Bruno Taccardi
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    - Lucas Lorenzo
  - CDSP
    - Dana Brooks
    - Ghandi Ahmad
- [www.cvrti.utah.edu/~macleod](http://www.cvrti.utah.edu/~macleod)  
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