

Appearance Changes in Image Registration

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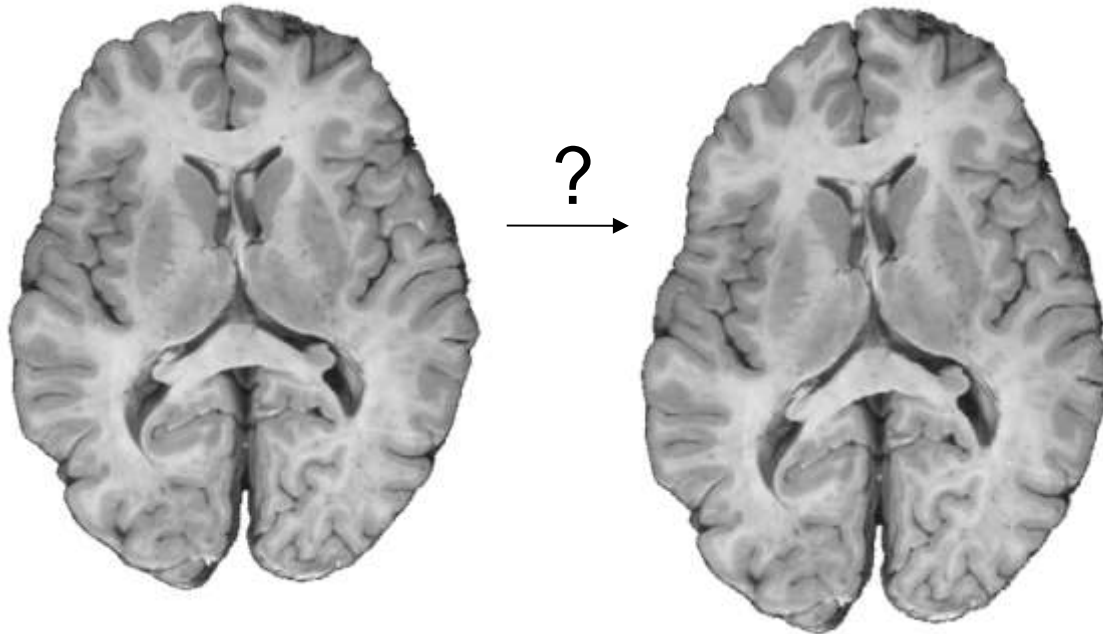
Warning



This talk is about approaches I have personally been involved with. Other people have been working in this area also and I will not do proper justice in terms of referencing.

Image Registration

Goal: Spatial alignment of two images



Source Image

Target Image

minimize Irregularity of transformation + image mismatch

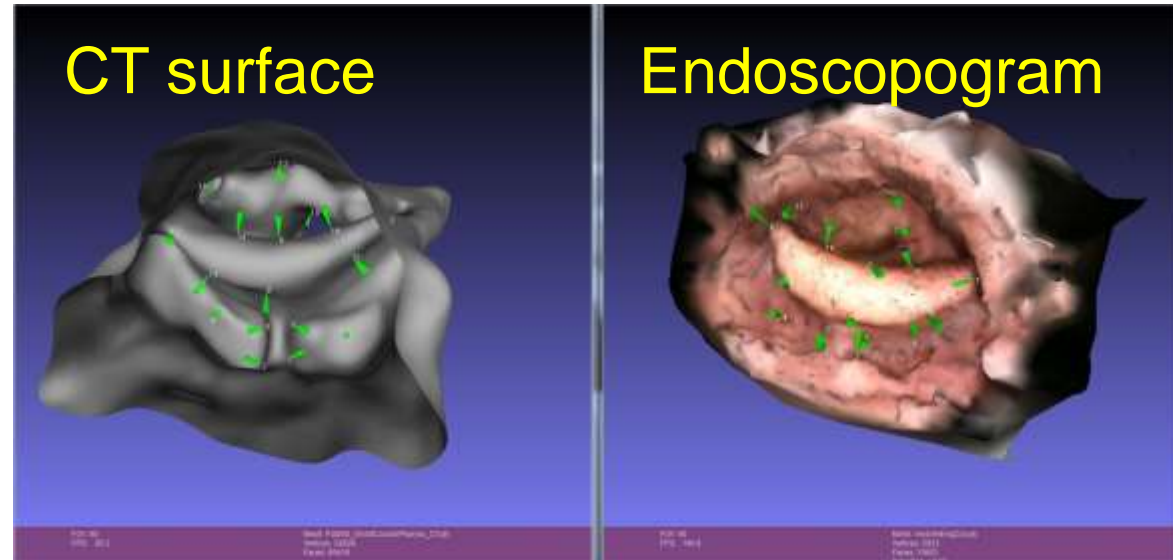
Sounds simple enough ...

The MD's perspective

Example Goal: Combine endoscopy and CT images
for improved cancer treatment planning.

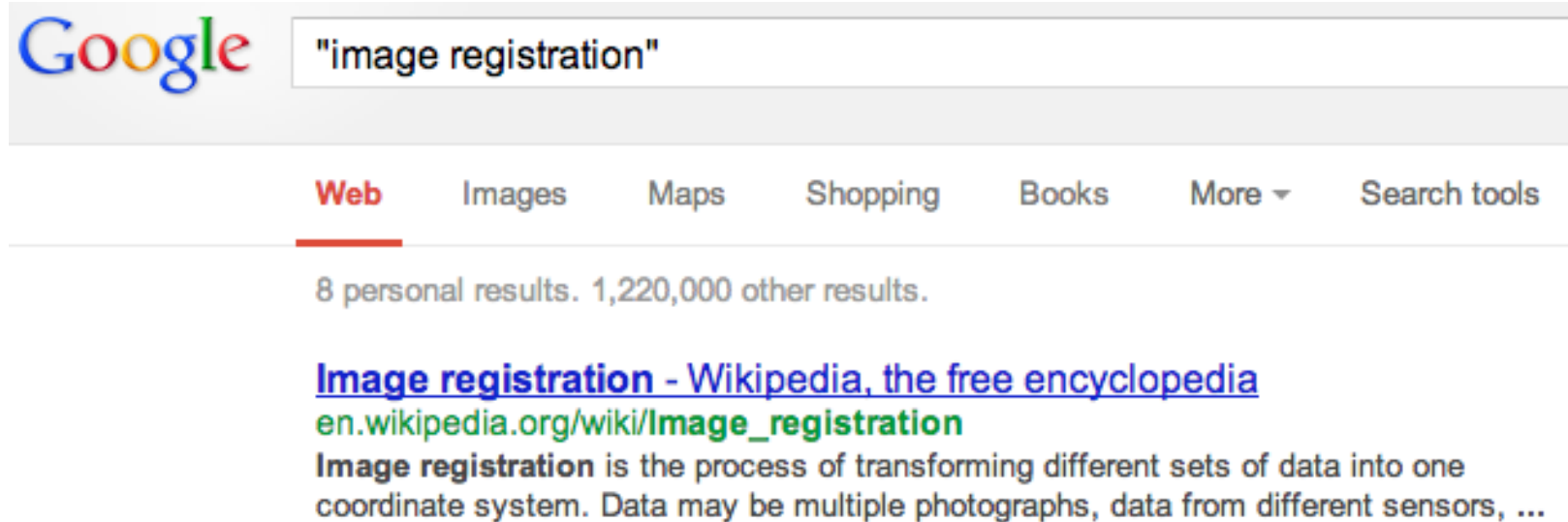


Julian Rosenman, MD



Approach: Registration (=spatial alignment)

The MD's perspective



A millions hits. "This is probably a solved problem."

The MD's perspective

The screenshot shows the NITRC website interface. At the top, the NITRC logo is on the left, followed by the tagline "The source for neuroimaging tools and resources". To the right is a search bar containing "image registration" and a "GO" button. Below the search bar are links for "Member login", "Register", "Help", "Share", and social media icons. A banner below the search bar states "NITRC Computational Environment is now available on Amazon Marketplace. Check it out!". On the right side of the banner, it says "Select Language" and "Powered by Google Translate".

Below the banner, there are two tabs: "Tools/Resources" (selected) and "Related Web Pages". To the left of the main content area is a sidebar titled "Narrow your results:" with a dropdown menu for "Domain". The dropdown is open, showing "MR (47)", "Domain Indepen...", and "PET/SPECT (5)".

The main content area shows the search results for "image registration". It includes a "Search within results:" input field, a "SEARCH" button, and a "Search Builder" link. Below this is a "Select All / Unselect All" link, a "Compare" button, and a "Sort by:" dropdown menu set to "Relevance". To the right of the sorting options is a "Results per page:" dropdown menu set to "20". At the bottom right of the results area, it says "Showing 1-20 of 52 results" with a red circle around the number "52" and a red arrow pointing to it. Below this are pagination links "1 | 2 | 3".

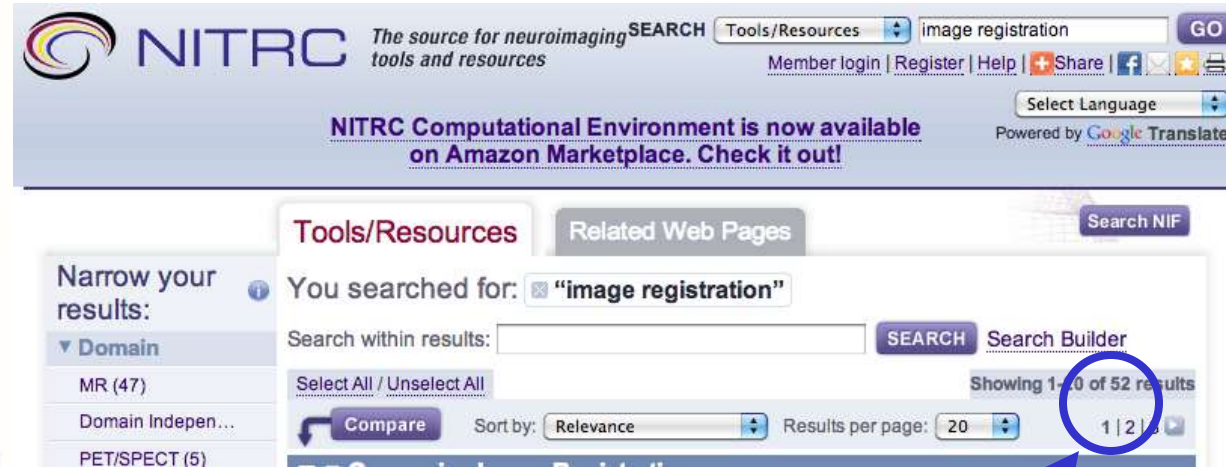
now we are down to 52 results

“Certainly 52 solutions to my problem are enough.”

The MD's perspective



Image: www.shapingyouth.org



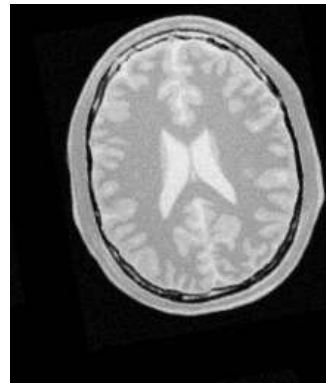
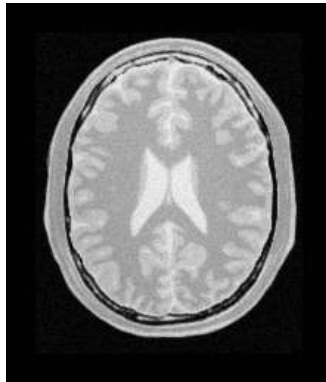
now we are down to 52 results

A closer look reveals:
*None of these programs
solve this problem.*

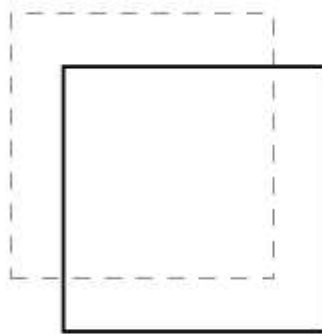
The sad reality: with a bit of hyperbole

Registration works really well when there is not much to register!

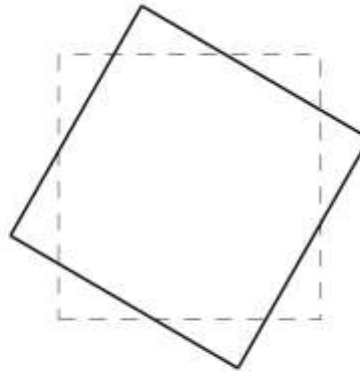
Similar
images



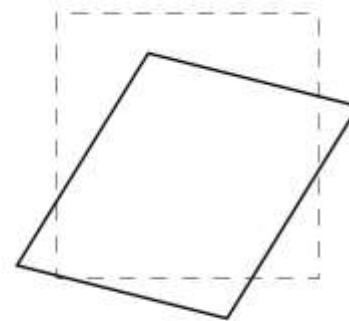
Simple
transforms



Translation
 $f : x \mapsto x + t$



Similarity Transform
 $f : x \mapsto sRx$

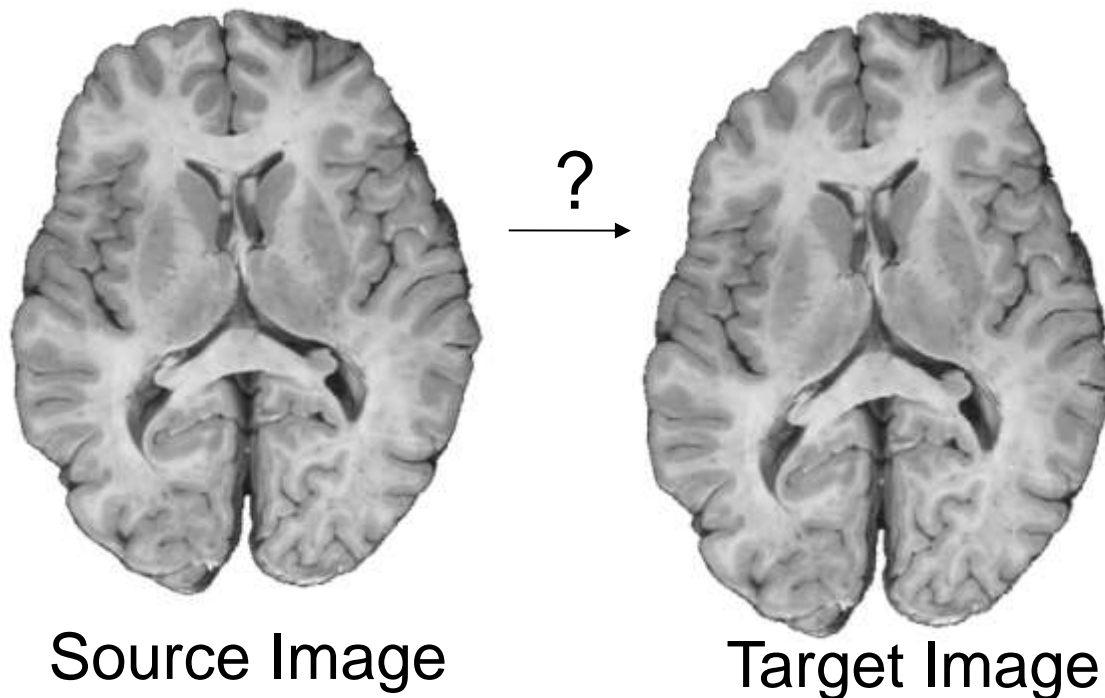


Affine Transform
 $f : x \mapsto Ax + t$

**However, in reality deformations are often more complex.
→ Need for general deformable registration methods.**

Deformable Image Registration

Goal: Spatial alignment of two images (beyond affine)
... for example to capture changes over time as in STIA ...



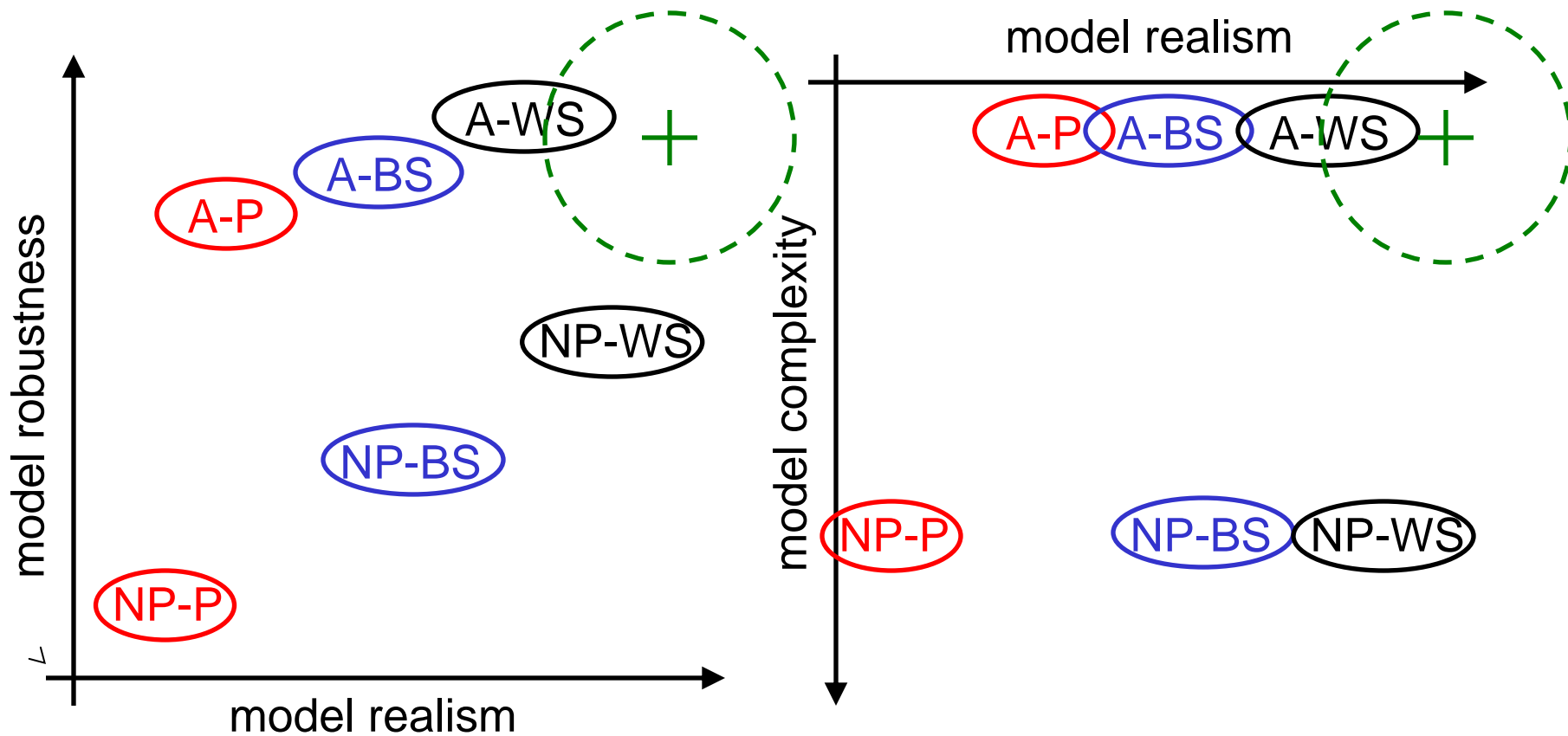
minimize Irregularity of transformation + image mismatch

Why is this hard?

Why is Deformable Image Registration Hard?

A: affine, **NP:** non-parametric (elastic, fluid, ...)

Within subject (**WS**); between subject (**BS**); with pathology (**P**)



Why is Deformable Image Registration Hard?

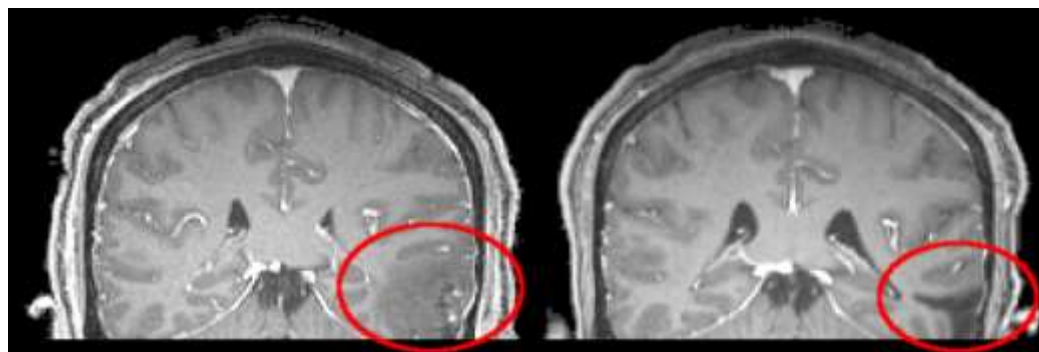
Problem 1: Unsuitable deformation models



Does your brain, leg, heart, ...
behave like a fluid?

Should it between two subjects?

Problem 2: Unsuitable similarity measures

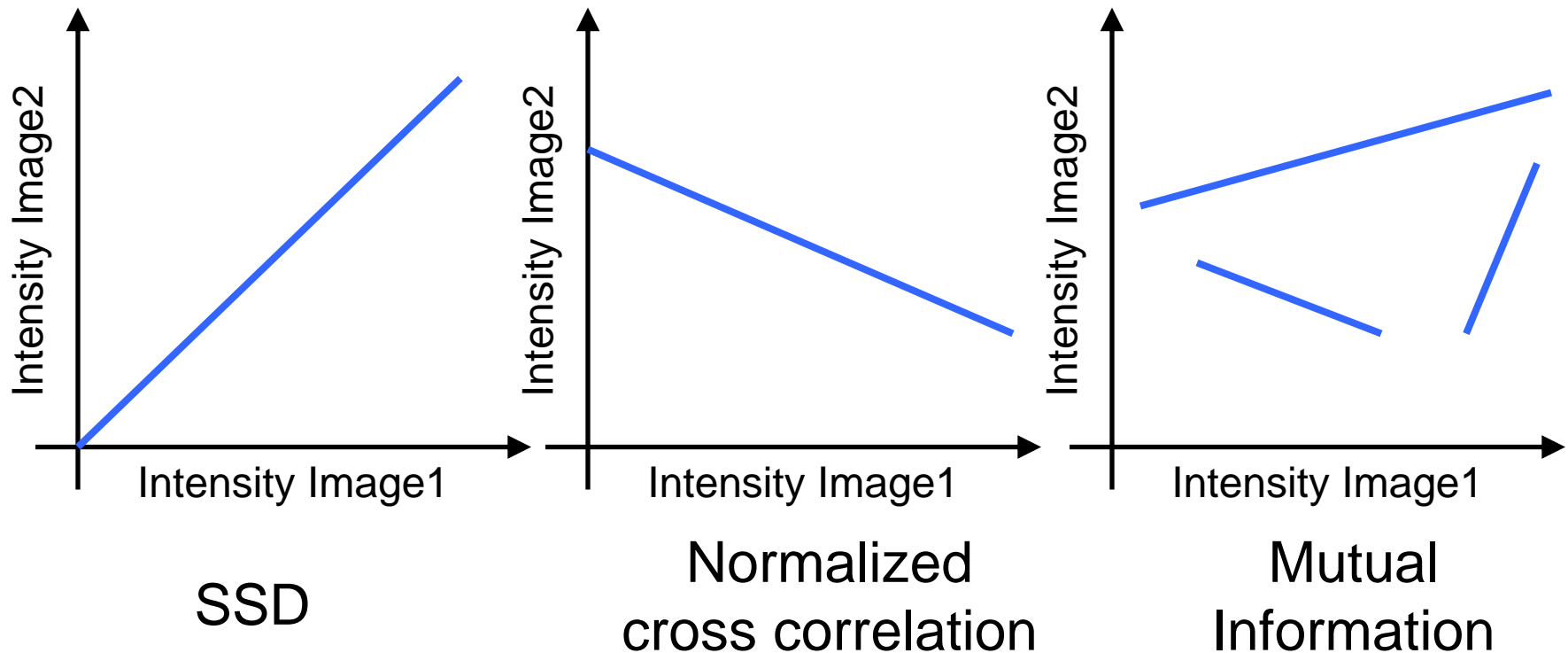


What if images have
different appearances?

Problem 3: Unsuitable numerical solutions

Basis of Similarity Measures

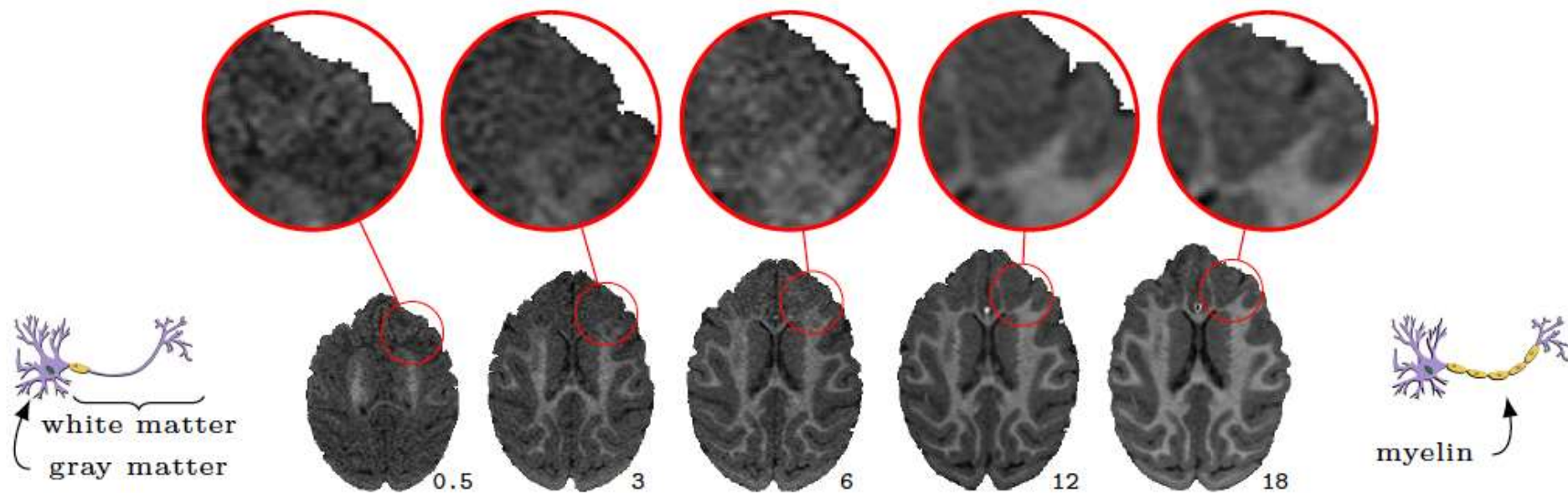
What is considered similar?



But sometimes correspondences are not quite so easy ...

Motivating issue 1: Intensity changes over time

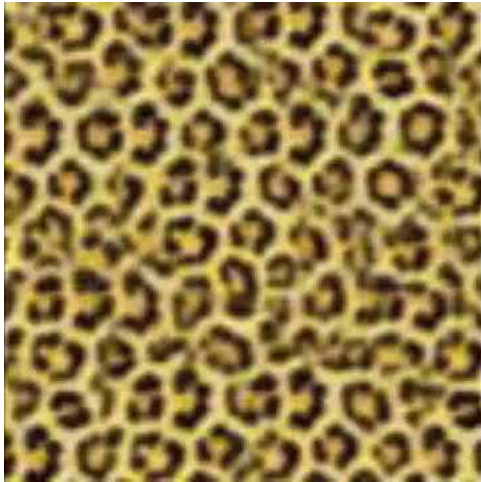
Normal brain development (macaque)



Locally changing image intensities cause problems for image similarity measures (SSD, mutual information, ...)

Motivating issue 2: Texture-blending

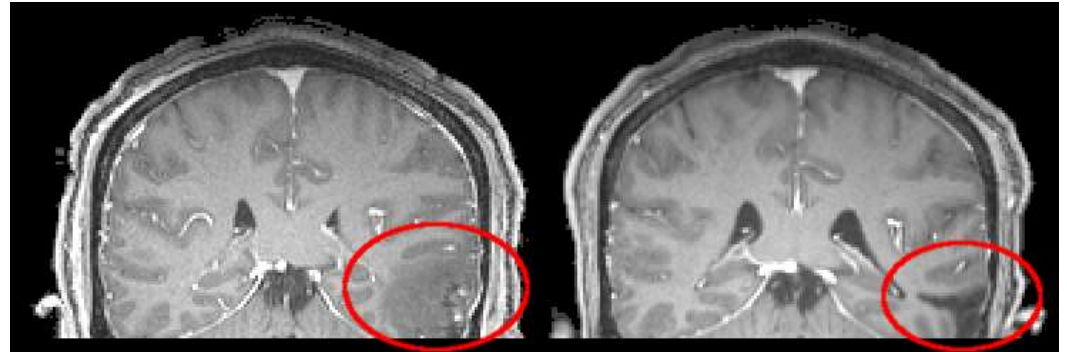
Texture blending for computer graphics.



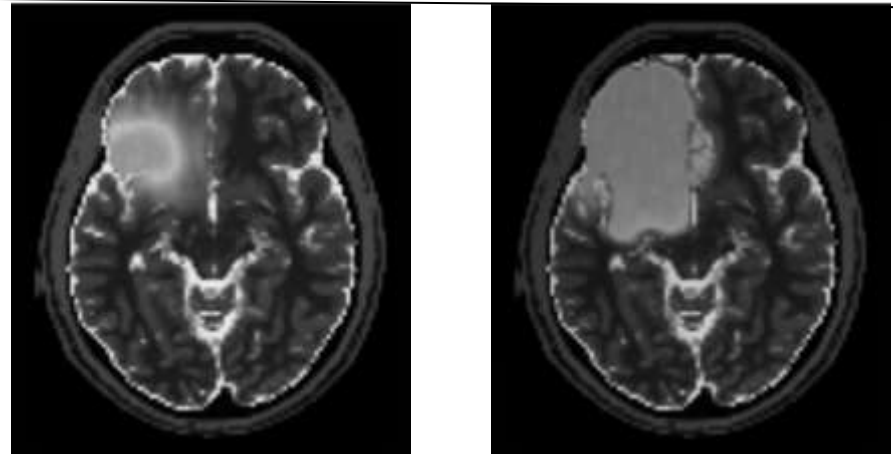
Extreme case: images are vastly different.

Motivating issue 3: Intensity/Structural changes

Traumatic brain injury
(real data)



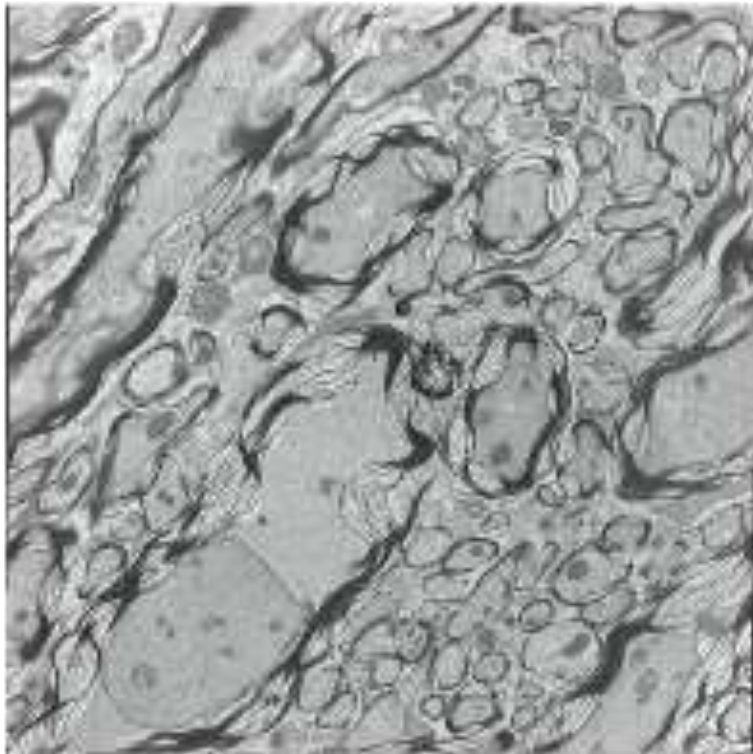
Brain tumor
(simulated data)



“Similar looking regions” do not correspond.
Structures only exist in one of the two images.

Motivating issue 4: Multimodal Registration

Electron microscopy



Light microscopy

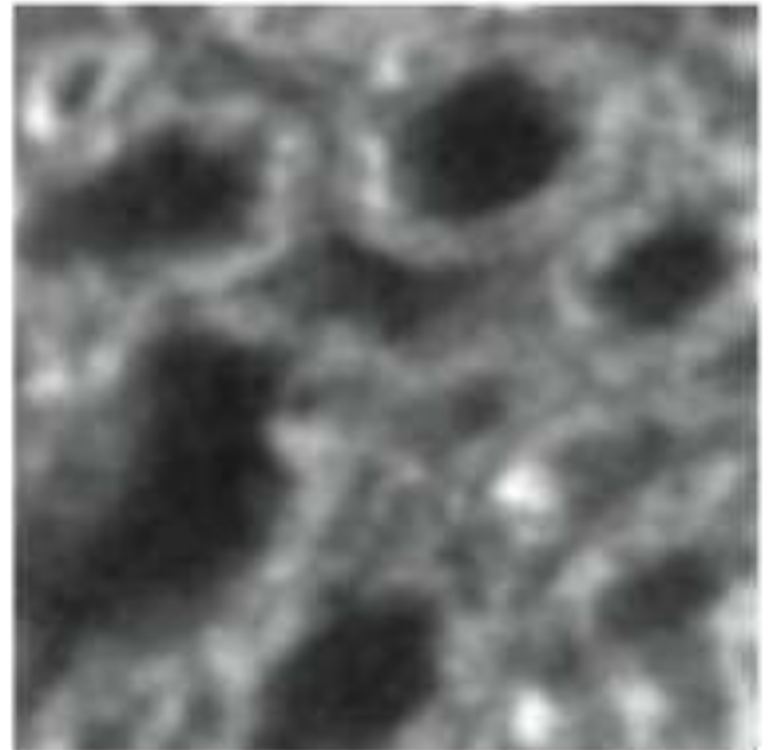


Image intensities differ, but additional complexities such as blurring are present and need to be accounted for.

What to do?

Is all hope lost here?

Possible Solutions

(Non)parametric modeling

VS

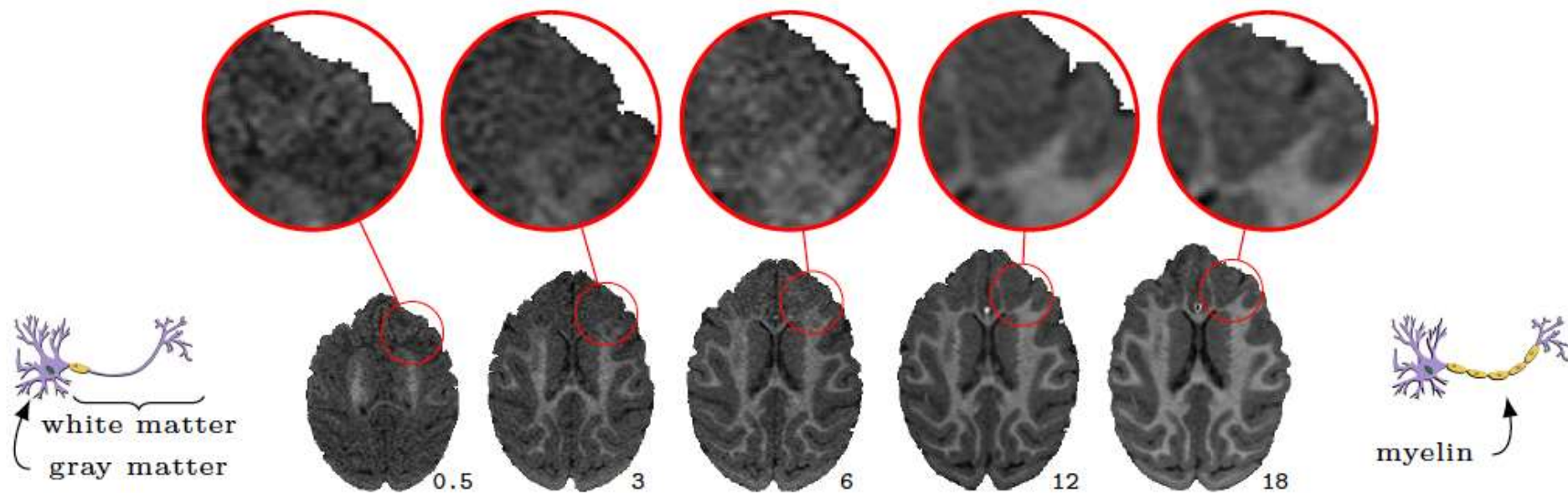
Data-driven approaches

Possible Solutions

Parametric Modeling

Motivating issue 1: Intensity changes over time

Normal brain development (macaque)

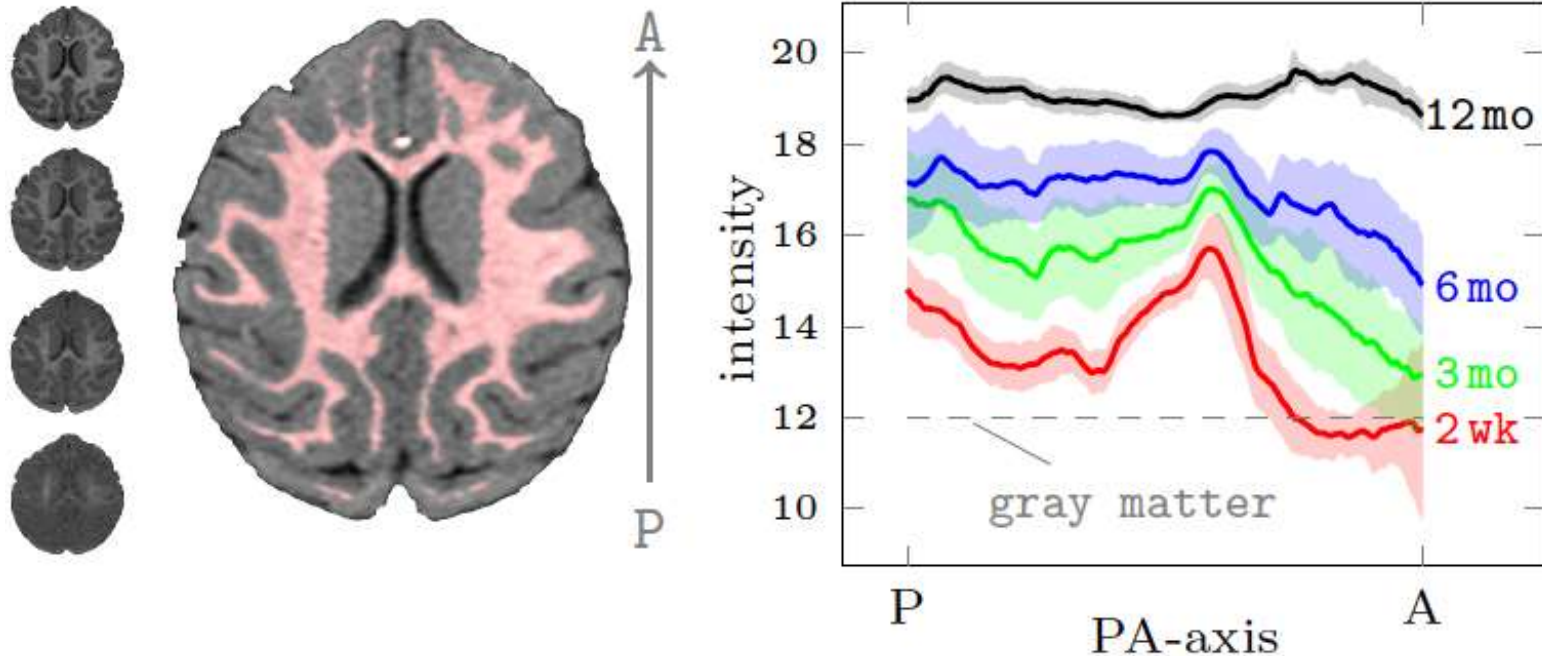


Possible solution:

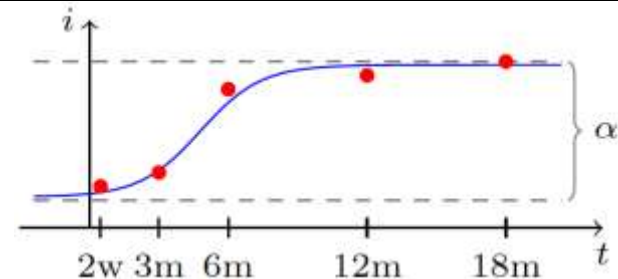
Impose a model over time to change your similarity measure

Modeling of Appearance Changes

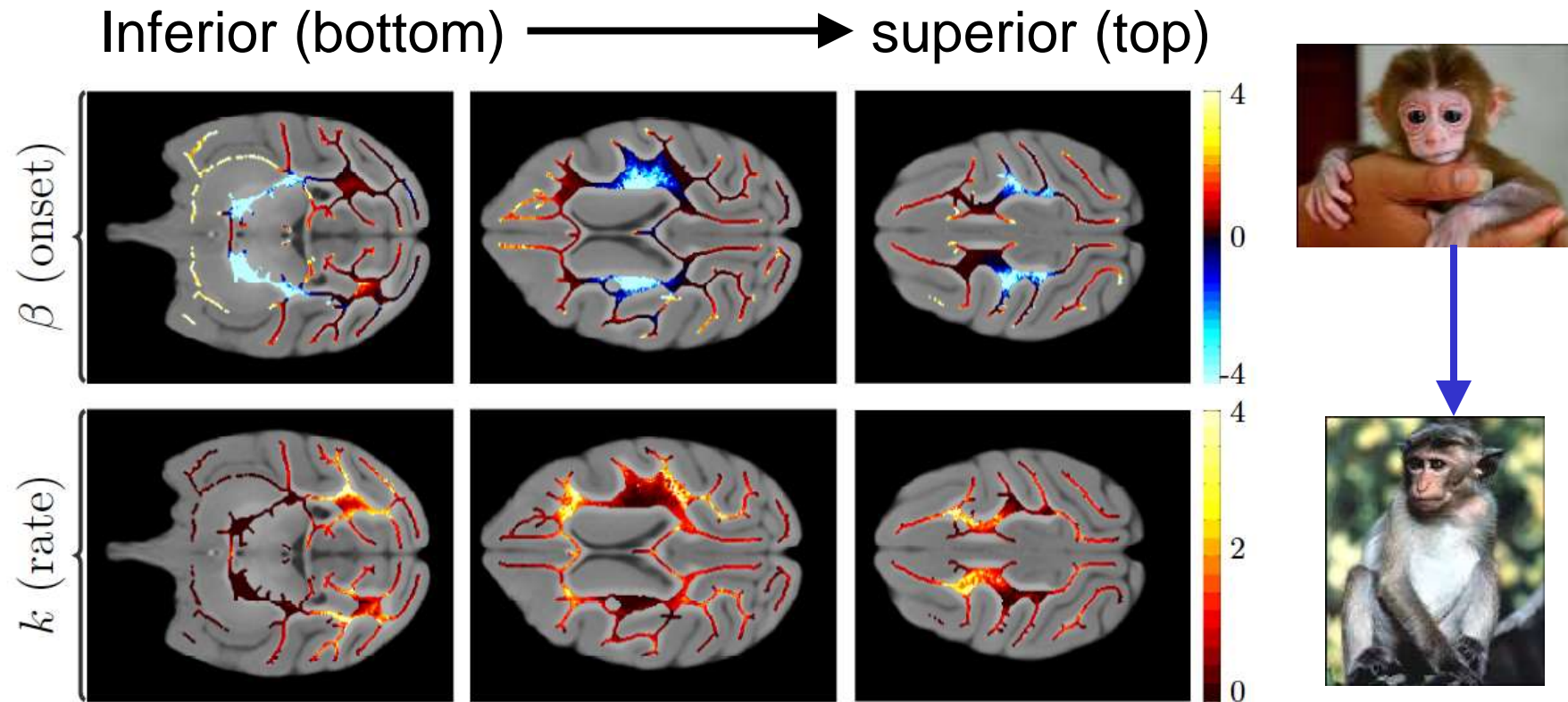
Normal temporal change (for a macaque monkey)



Concretely: Impose logistic model
[your favorite model] to account
 for expected changes over time



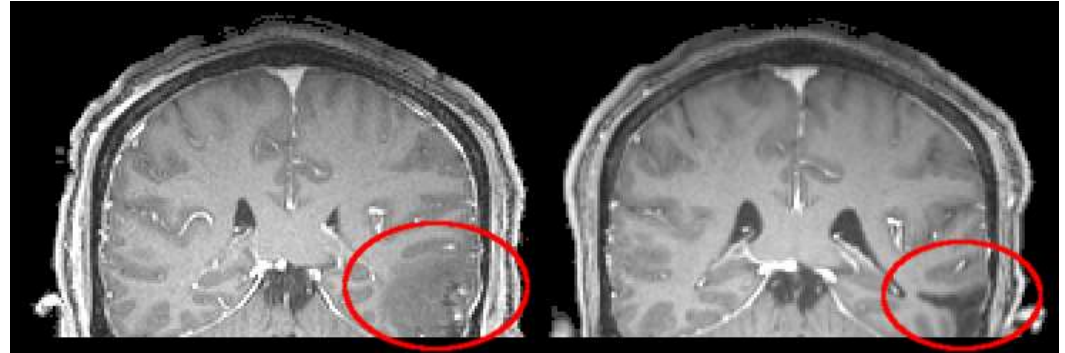
Appearance Change: Brain Development



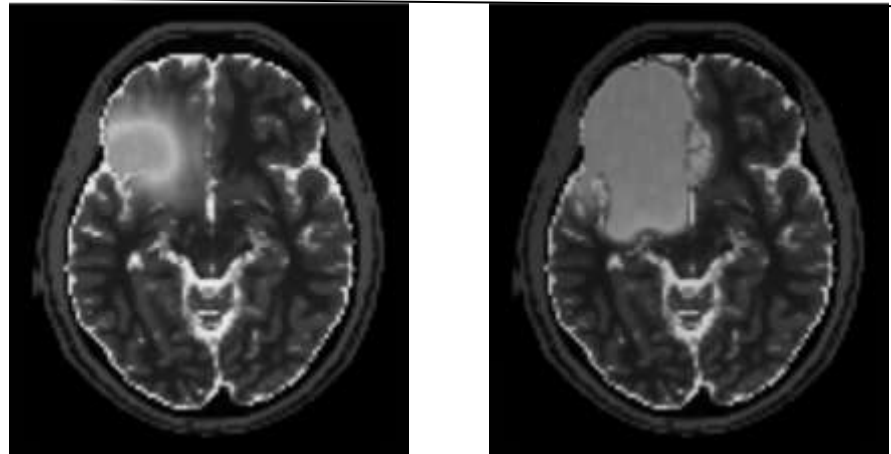
This strategy not only allows for improved registration results, but also provides interesting information about the general brain maturation process ...

What do we do with non-corresponding regions?

Traumatic brain injury
(real data)



Brain tumor
(simulated data) –
TumorSim [Prastawa et al.]

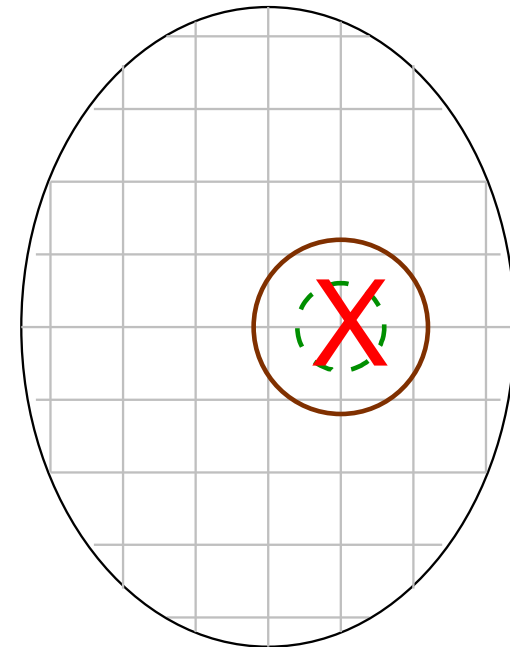


As we cannot match them we somehow need to
model or ignore the changes.

Solution 1: Cost-function masking

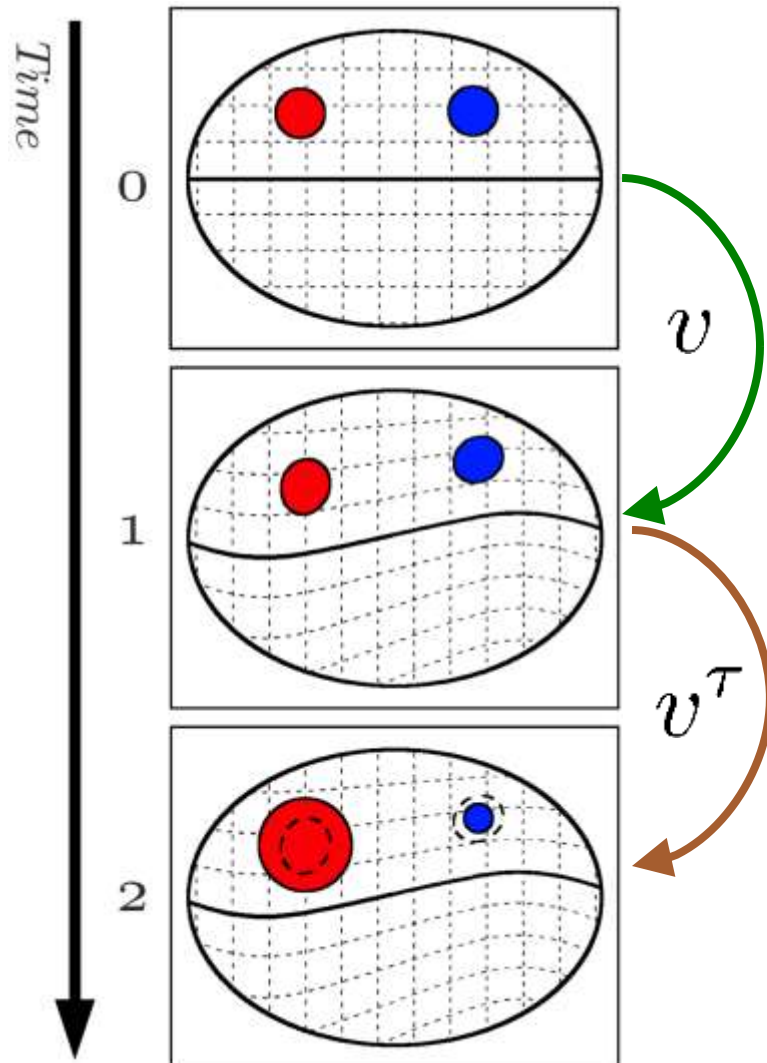
One solution: Cost function masking [Brett2001]

= ignoring matching cost in region of source image



... let's just not look at it!

Solution 2: Geometric Metamorphosis



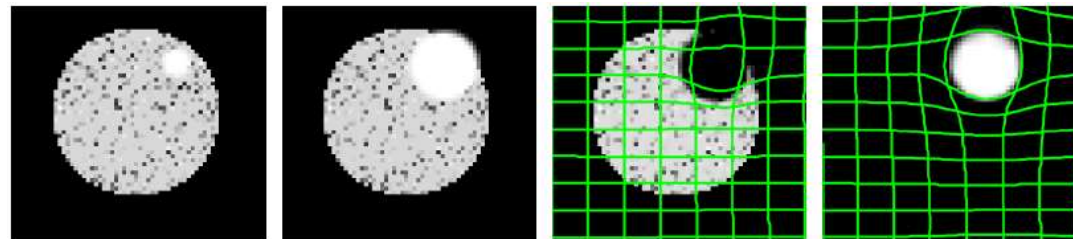
Model lesion/tumor/... and its temporal change

- **Composition of two deformations**
 - e.g., tissue displacement & infiltration
 - jointly estimated
- **Image composition model**
 - = “glorified cost-function masking”

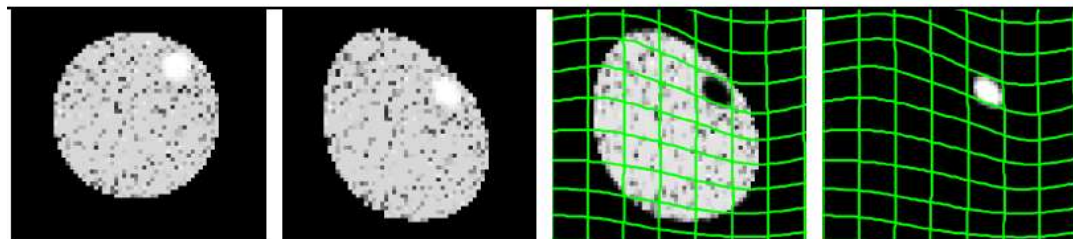
Model is probably more interesting from a *deformation modeling* perspective..

Geometric Metamorphosis: Synthetic Results

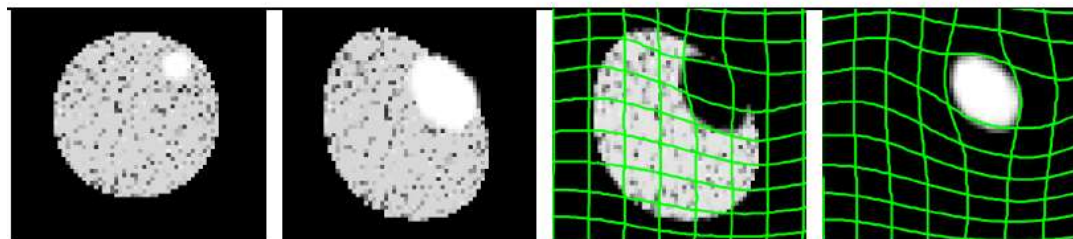
Only infiltration



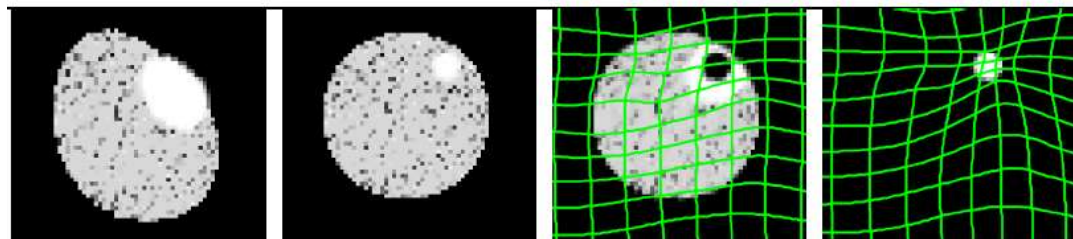
Only deformation



Deformation + infiltration

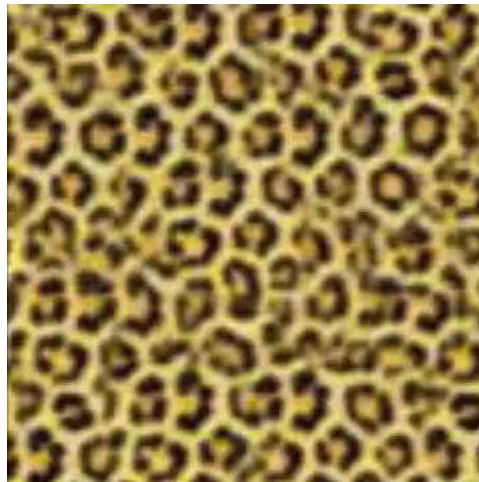


Deformation + recession



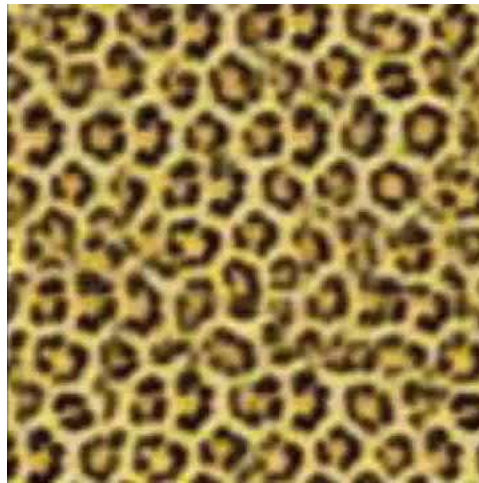
Possible Solutions

Non-parametric Modeling w/o learning to deal with very complex changes

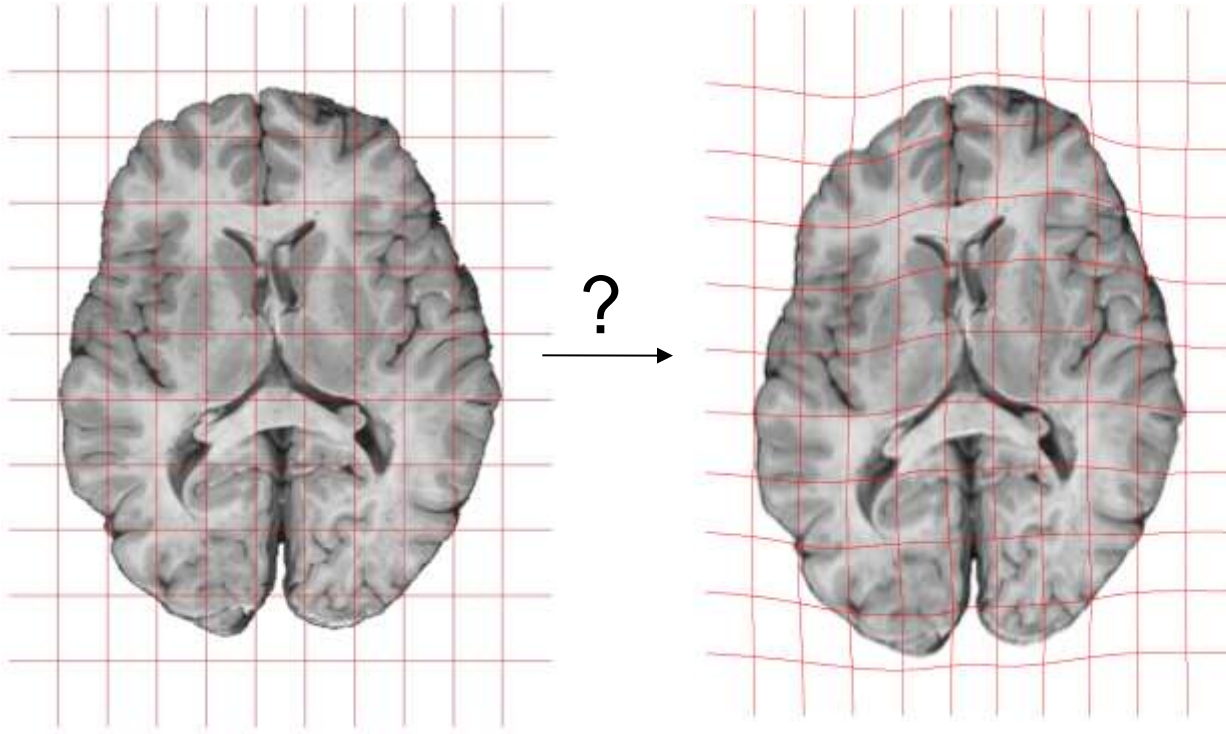


Possible Solutions

One solution is **metamorphosis**,
which requires a little LDDMM detour
[Miller, Trounev, Younes, ...]



LDDMM detour



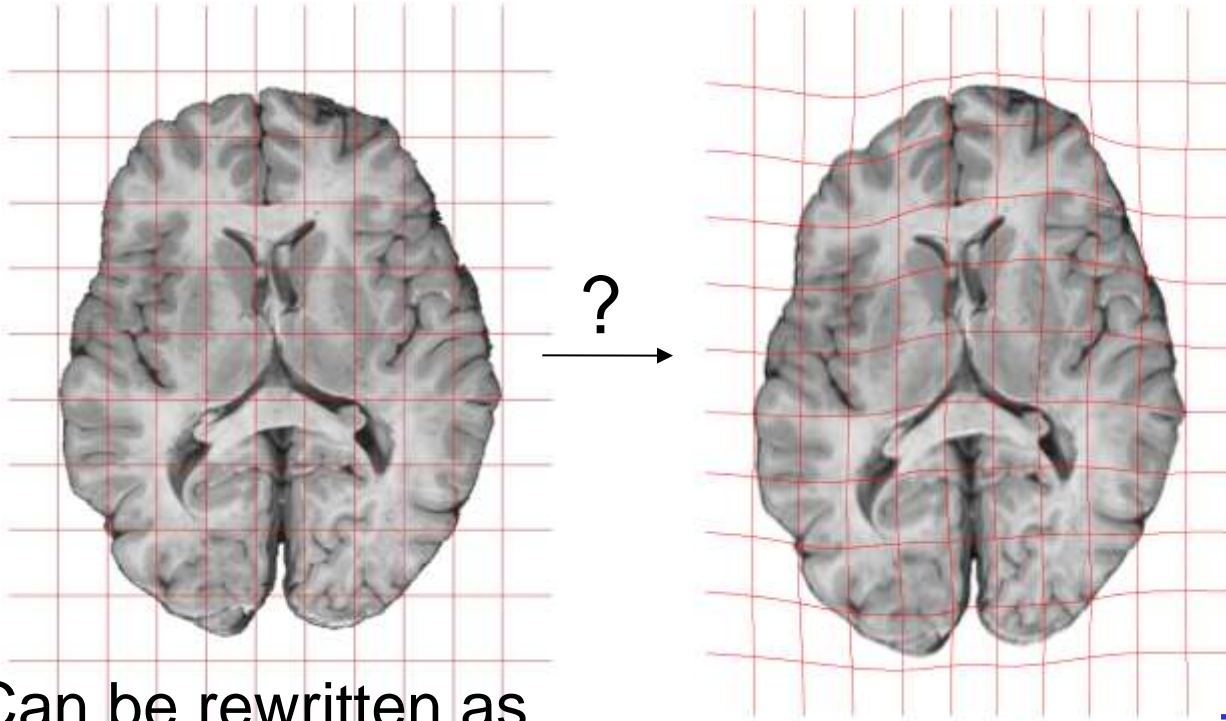
What is the best velocity field, v , to deform one image into the other?

Fluid flow setup [Miller, Younes, Trounev, ...]:

$$E(v, \Phi) = \int_0^1 \|v\|_V^2 dt + \frac{1}{\sigma^2} \|I_0 \circ \Phi_{1,0} - I_1\|_{L_2}^2 \quad \text{s.t.} \quad \dot{\Phi} = v \circ \Phi$$

Optimal control problem, which can be rewritten as ...

Constrained Optimization for LDDMM



Can be rewritten as

$$E(v, I) = \int_0^1 \|v\|_V^2 dt + \frac{1}{\sigma^2} \|I(1) - I_1\|_{L_2}^2$$

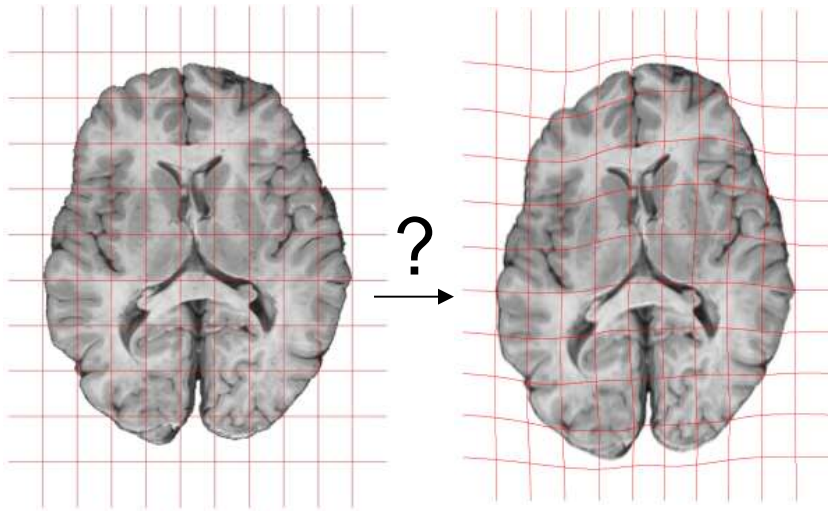
s.t. $I_t + \nabla I^T v = 0, I(0) = I_0$

This just requires
infinite-dimensional
constrained
optimization.

... and I am telling you this because ...

Image Registration + Image Metamorphosis

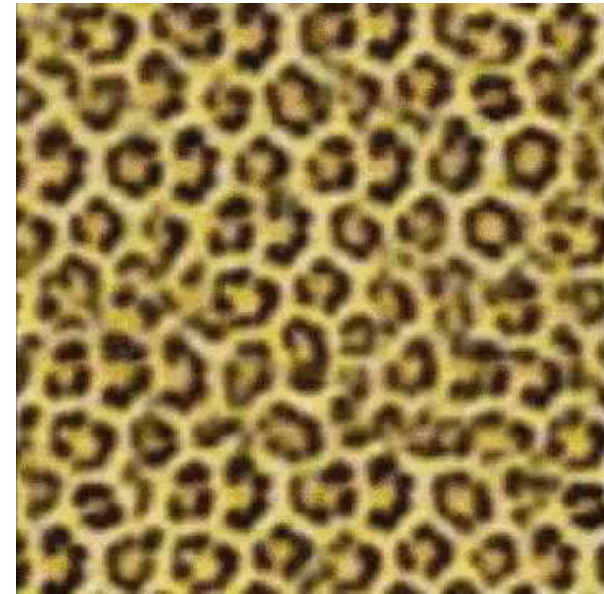
Standard Image Registration



$$I_t + \nabla I^T v = 0$$

Assumes **1-1 correspondence**

Image Metamorphosis



$$I_t + \nabla I^T v = q$$

Registration **and blending**

add $\int_0^1 \|q\|_Q^2 dt$ to energy

Image Metamorphosis

**Metamorphosis is an elegant model,
but work remains to be done**

- to improve the numerical solution methods
- to extend it to longitudinal data
- to possibly couple it with some parametric models for greater control over the appearance change

Possible Solutions

Let's switch gears a bit ...

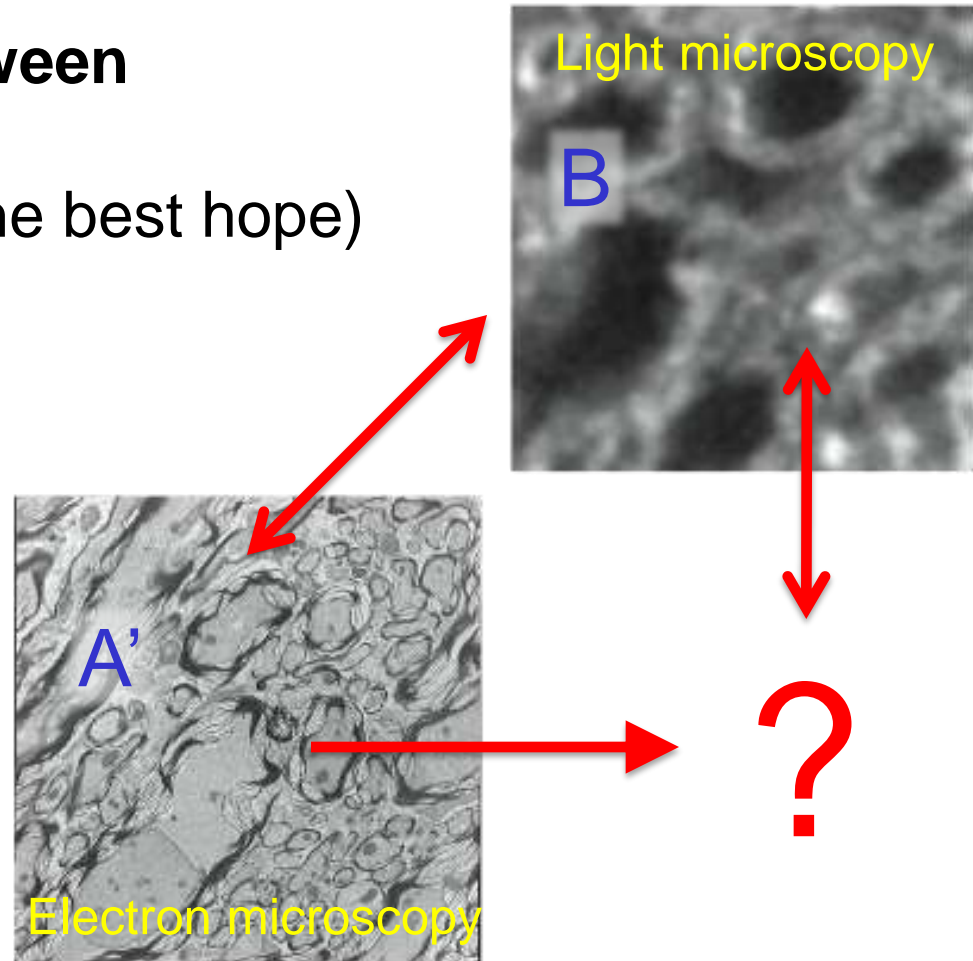
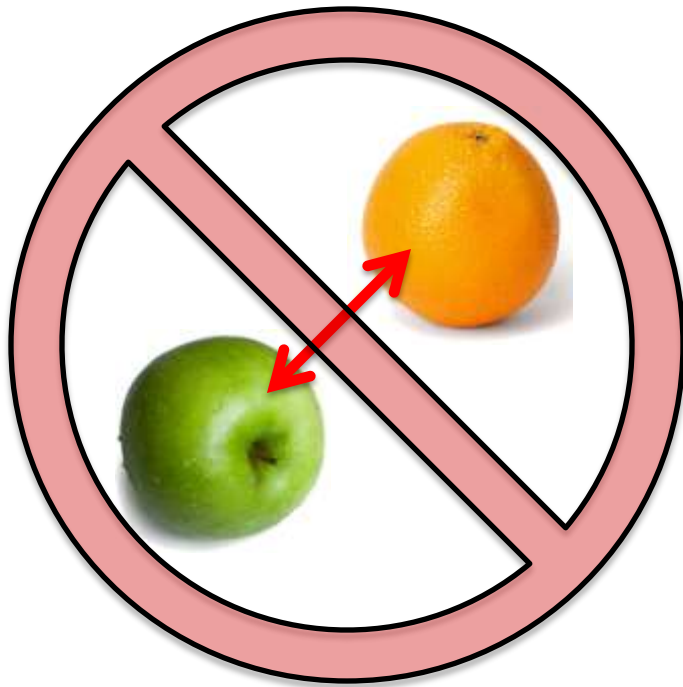
Data-Driven (Learning) Approaches

... will tell you about two different approaches:

1. Image analogies (for microscopy)
2. Recap of “Low-rank to the rescue”

Registration for Microscopy

Registration is difficult between different image modalities
(mutual information may be the best hope)



Other possible solution: Image Analogies (from graphics)

Registration for Microscopy: Image Analogies

Solution approach:

Image Analogies:



learned

A relates to B

A' relates to B'



unknown

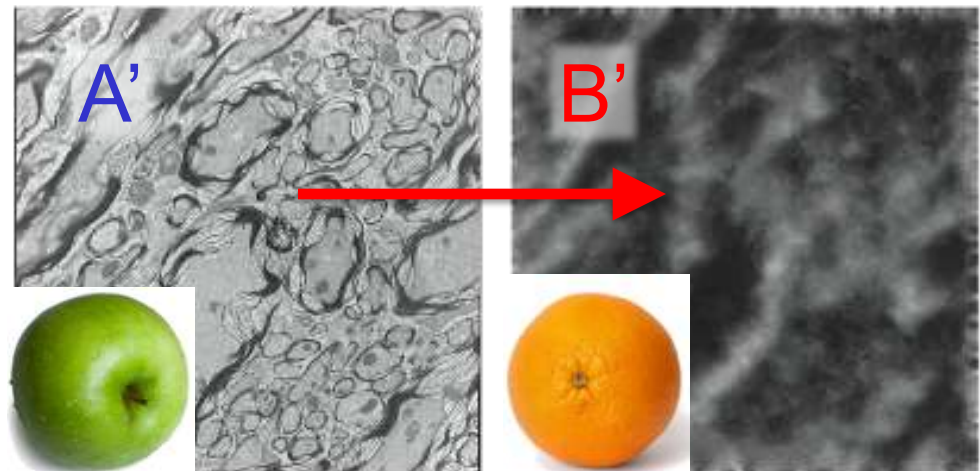
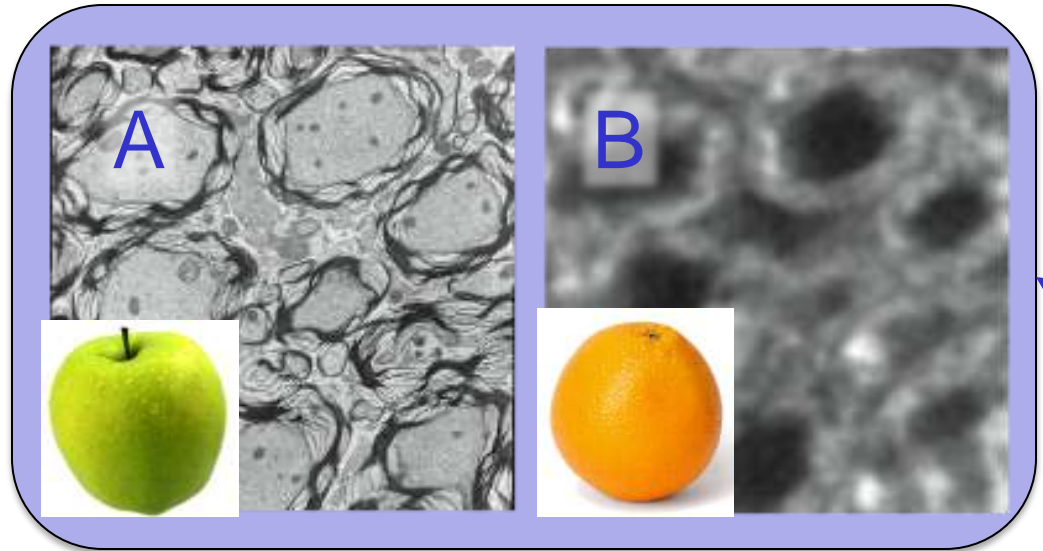


Image-Analogies by Lookup

**Generate corresponding
Image patches**

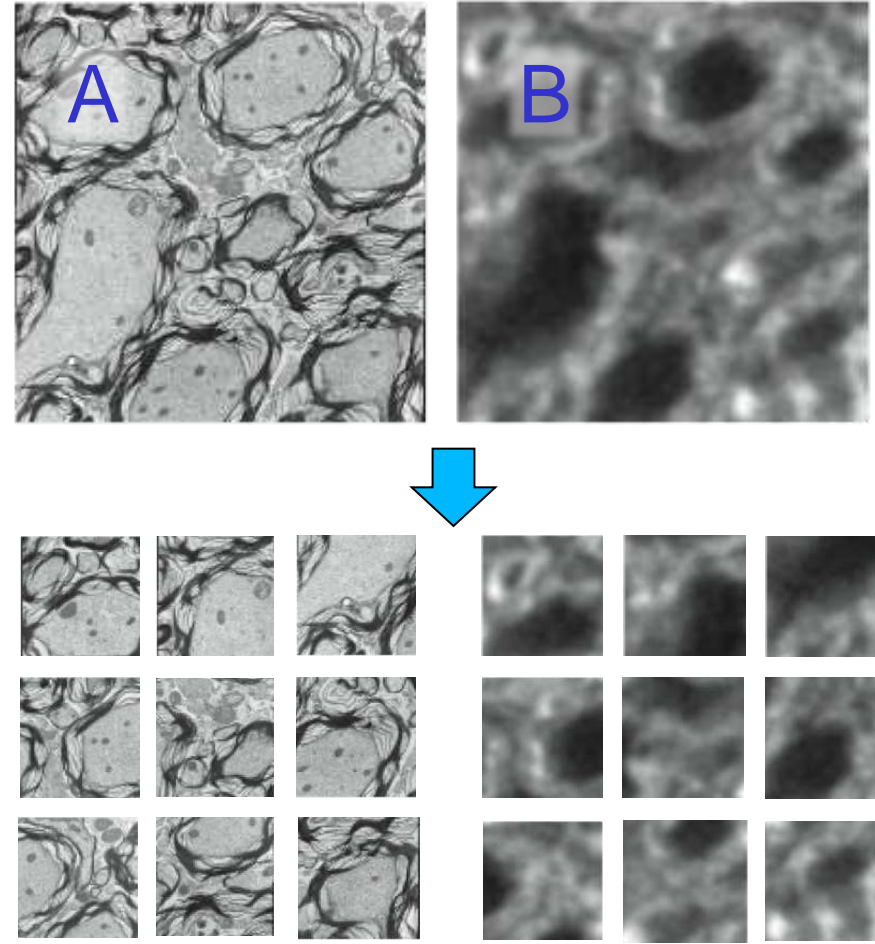


Image-Analogies by Lookup

**Synthesize a new image
by lookup**

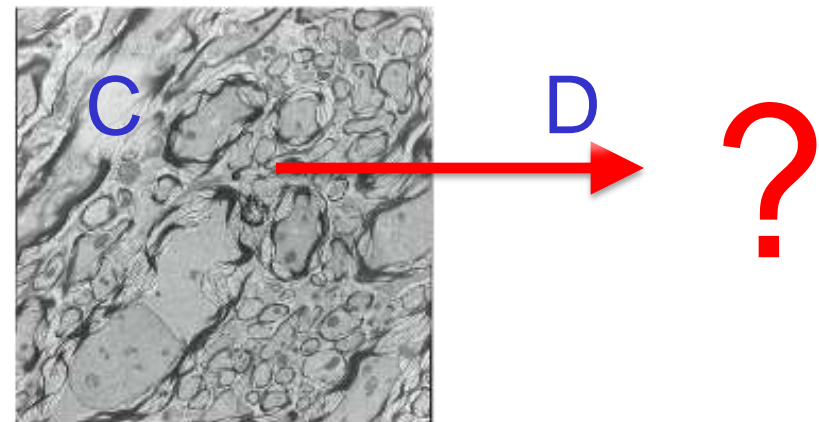
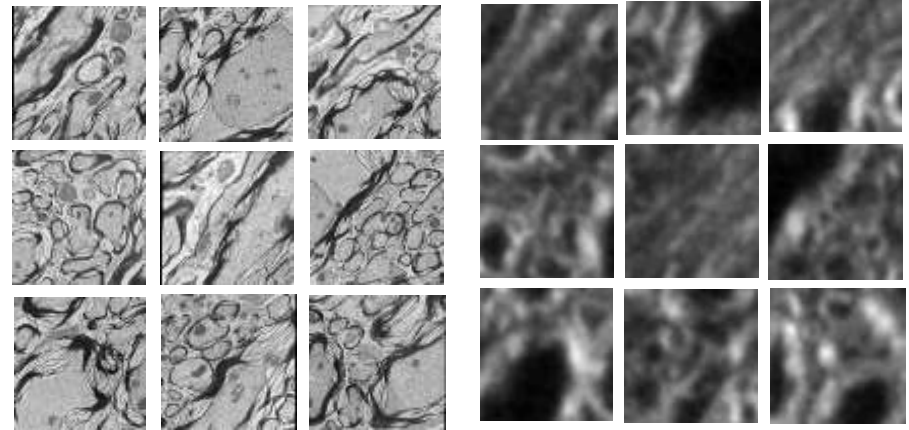


Image-Analogies by Lookup

**Synthesize a new image
by lookup**

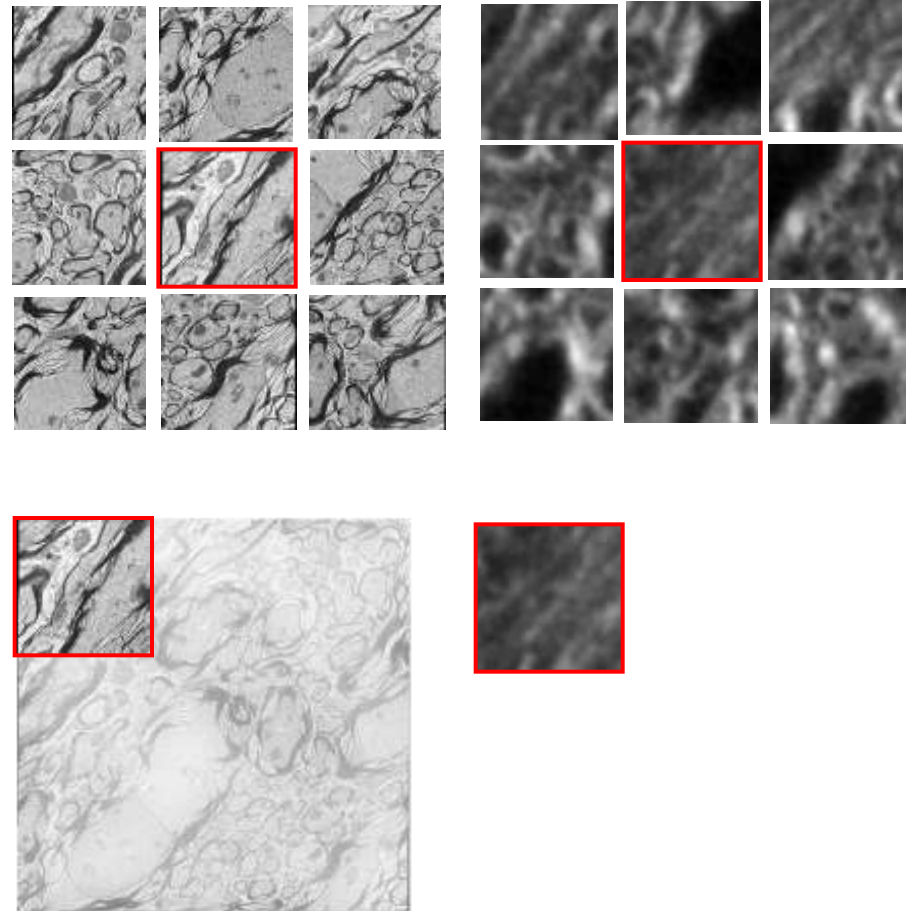


Image-Analogies by Lookup

**Synthesize a new image
by lookup**

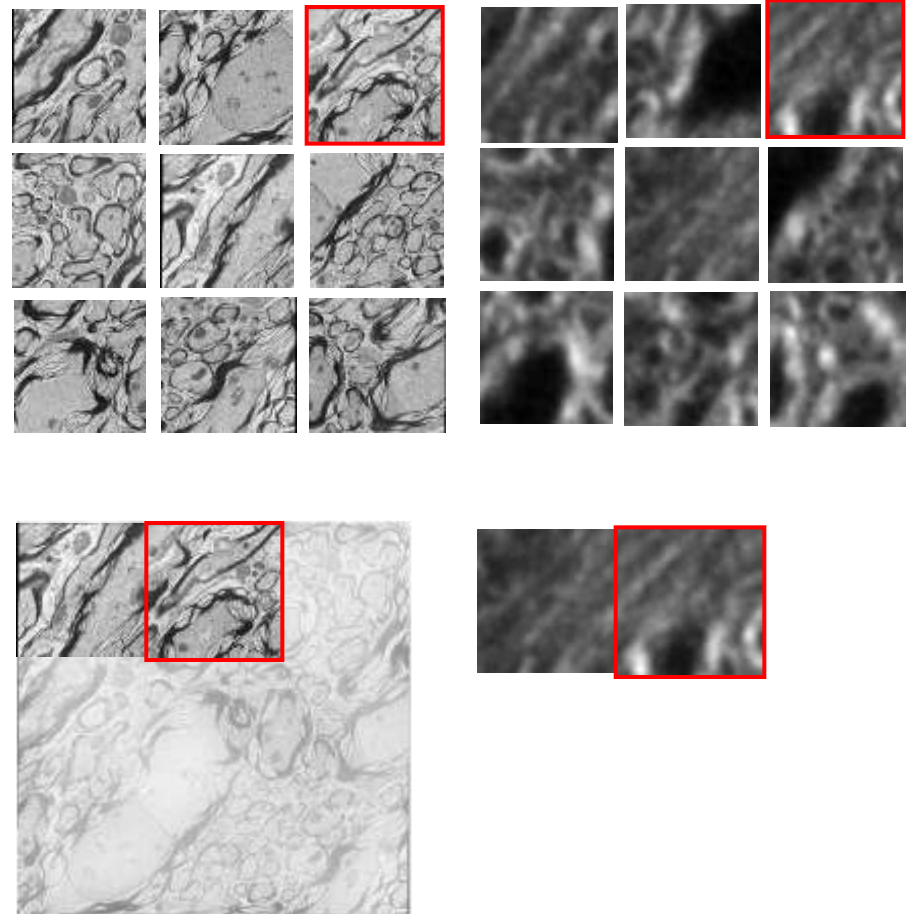


Image-Analogies by Lookup

**Synthesize a new image
by lookup**

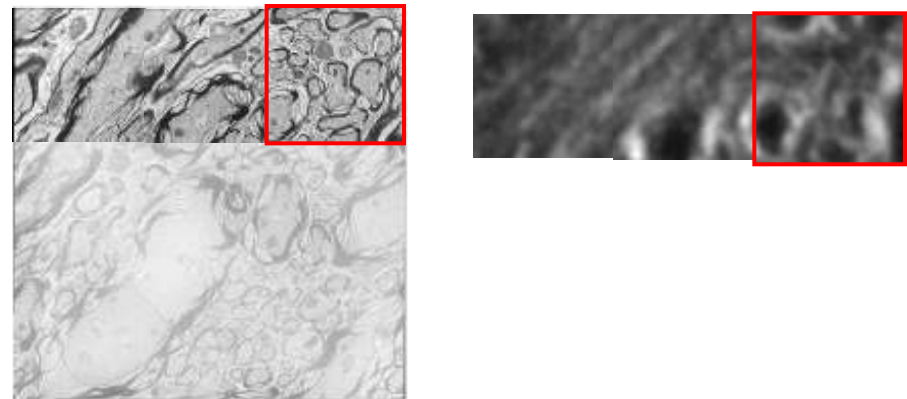
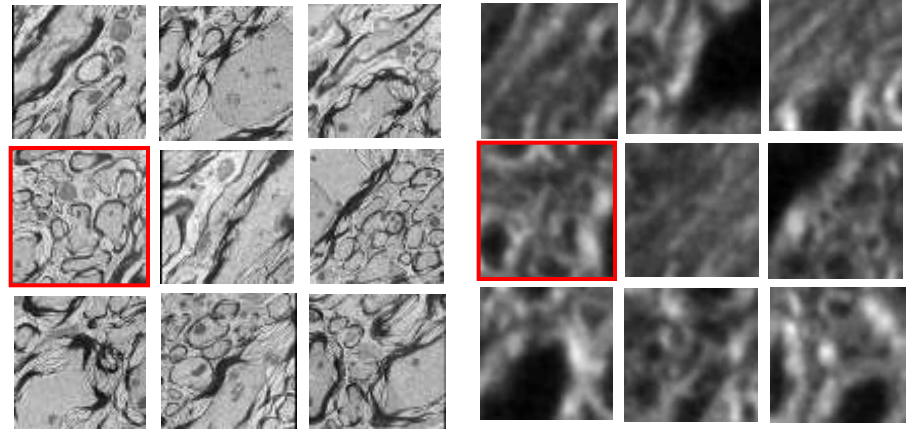


Image-Analogies by Lookup

**Synthesize a new image
by lookup**

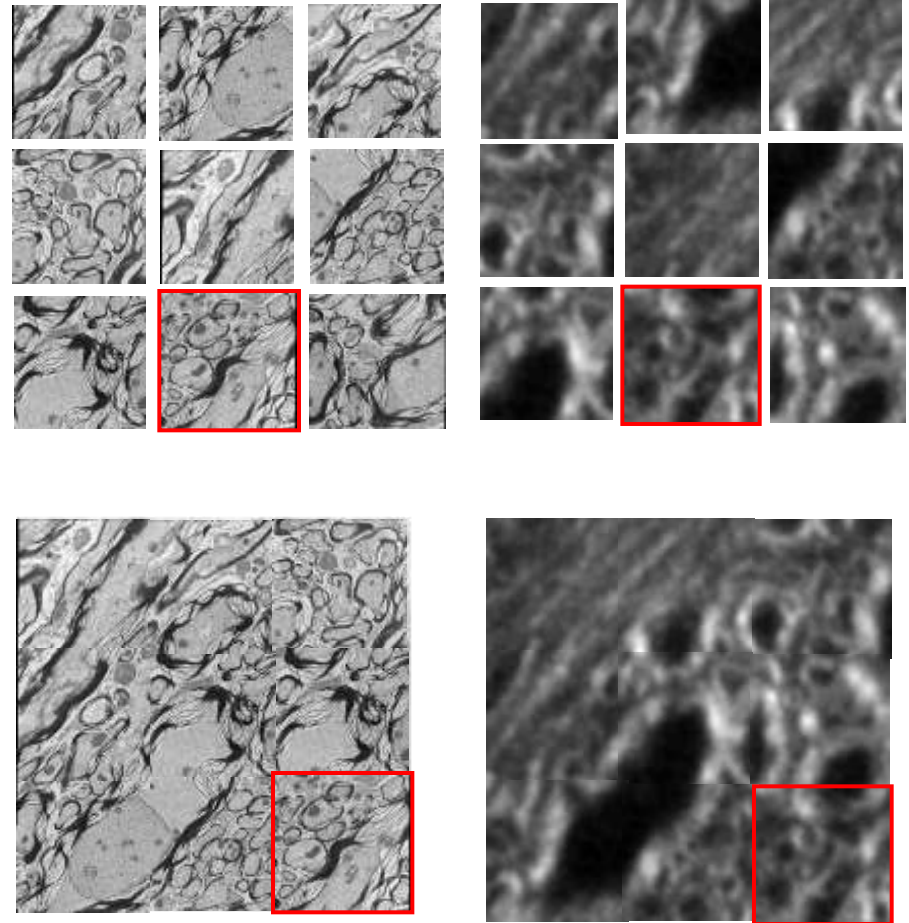
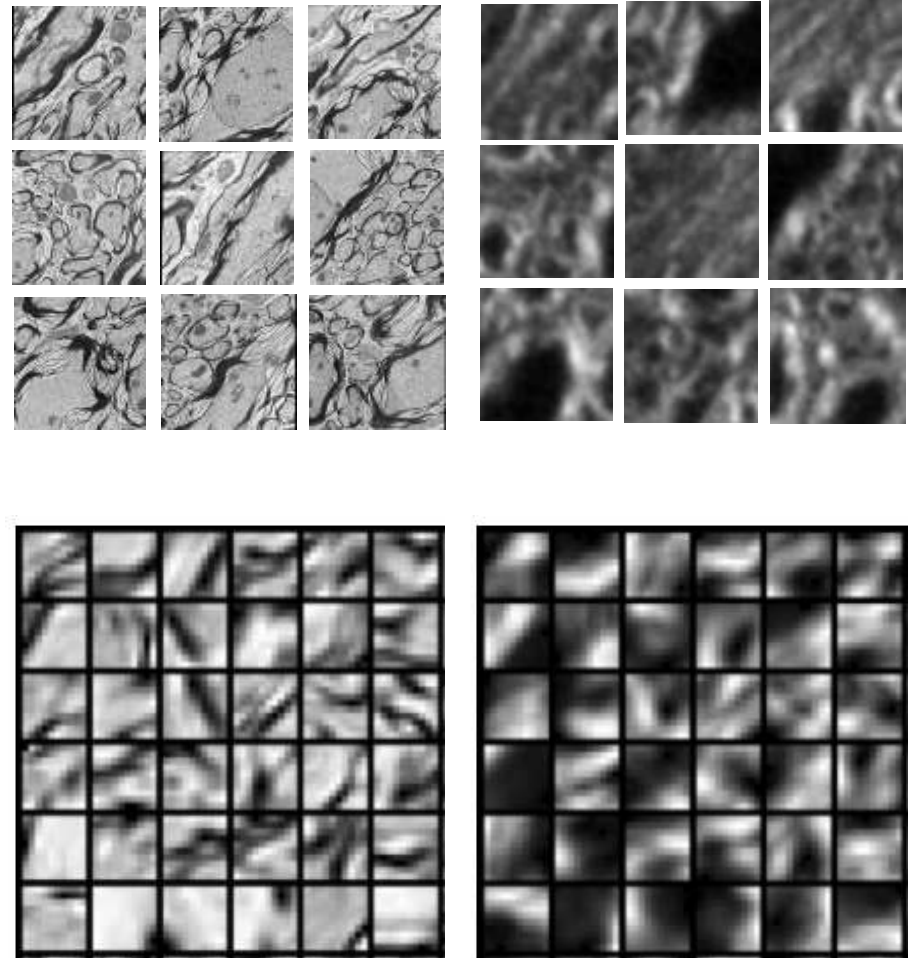


Image-Analogies by Dictionary Learning

Use **LASSO** for dictionary learning to learn a basis for patches which can be used to predict one modality from the other.



Possible Solutions

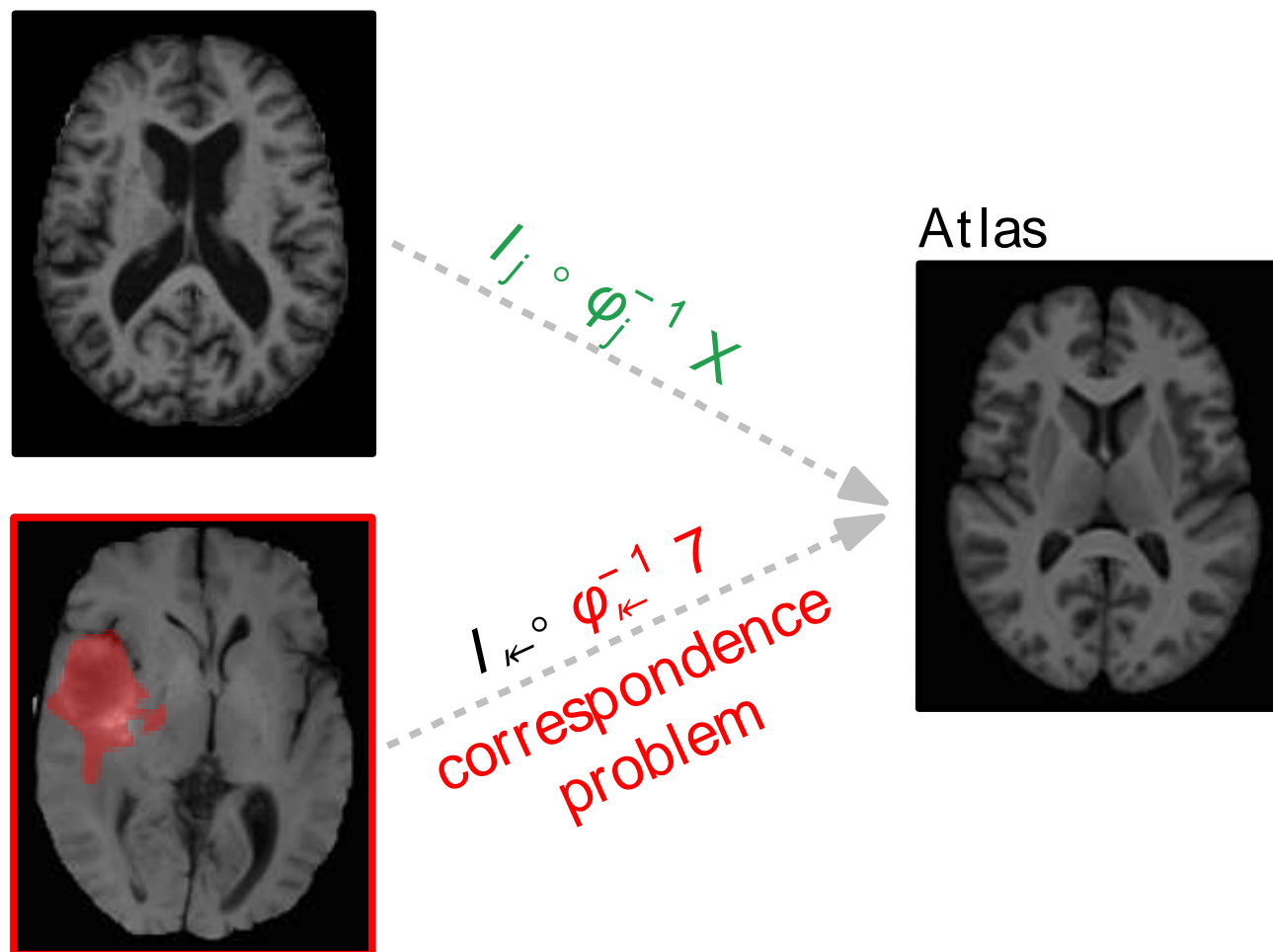
Learning from Populations

Super-brief summary of Roland Kwitt's talk from yesterday:

Low-rank to the rescue:

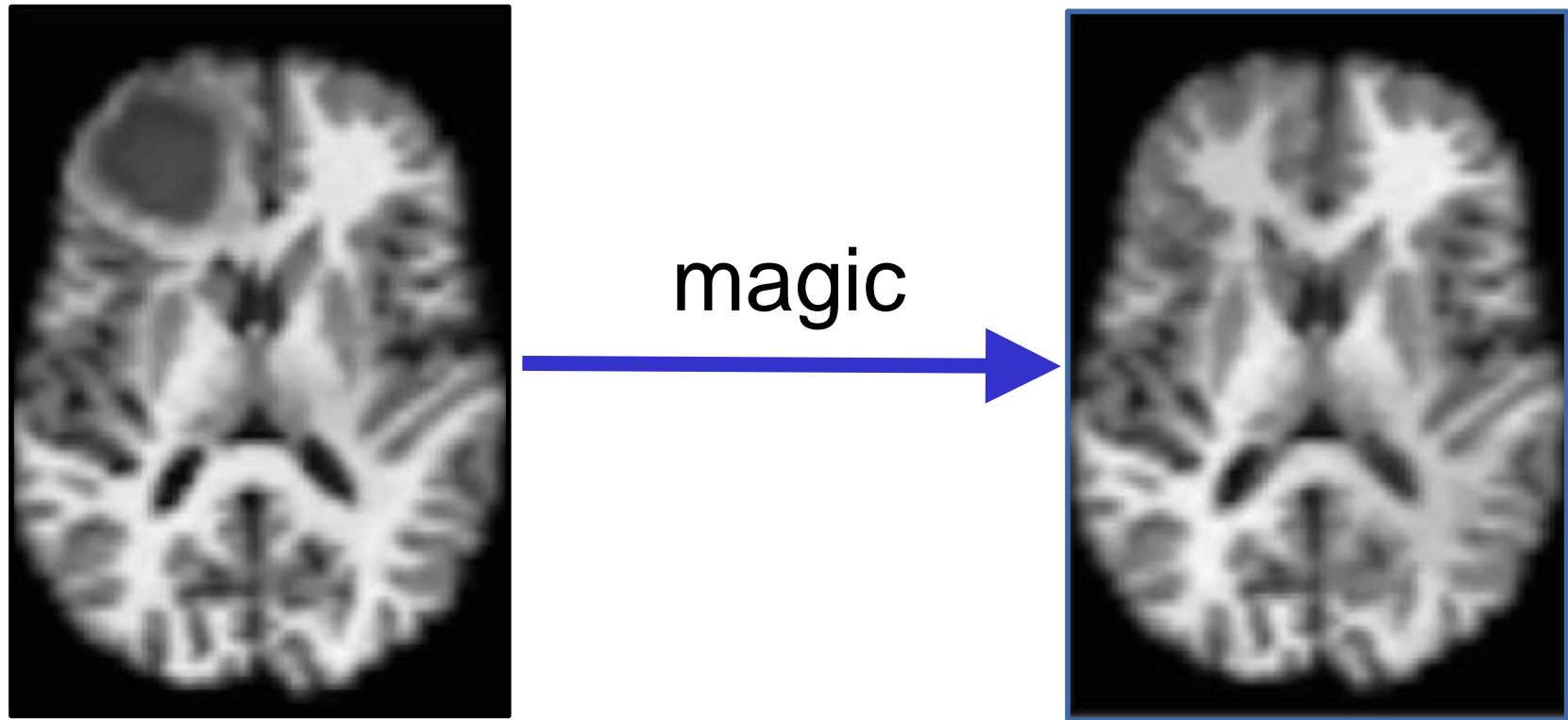
Atlas-Based Analyses in the Presence of Pathologies

Motivating Problem: Registration w/ Pathologies



What if?

What if there were a method to transform an image with pathology into a healthy-looking image?



This is exactly what “Low-rank to the Rescue” does!

Low-rank + sparse decomposition

$$\mathbf{C} = \left(\begin{array}{c} \xrightarrow{N} \\ \text{[Corrupted Image: Blue/Yellow/Red with noise]} \end{array} \right) = \left(\begin{array}{c} \text{[Clean Image: Blue/Yellow/Red]} \end{array} \right) + \left(\begin{array}{c} \text{[Sparse Noise Matrix]} \end{array} \right)$$

$\text{rank}(\mathbf{C}) = N$
Low-rank \mathbf{L}
($\text{rank}(\mathbf{L}) = 3$)
Sparse \mathbf{S}

$$\{\mathbf{L}^*, \mathbf{S}^*\} = \underset{\mathbf{L}, \mathbf{S}}{\operatorname{argmin}} \underbrace{\|\mathbf{L}\|_*}_{\text{low-rank}} + \lambda \underbrace{\|\mathbf{S}\|_1}_{\text{sparsity}}, \text{ s.t. } \mathbf{C} = \mathbf{L} + \mathbf{S}$$

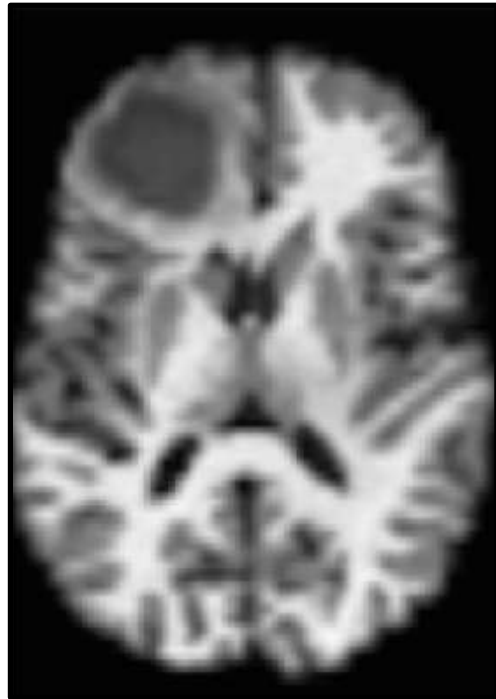
Low-rank + sparse decomposition for images

Images are represented by column-vectors.

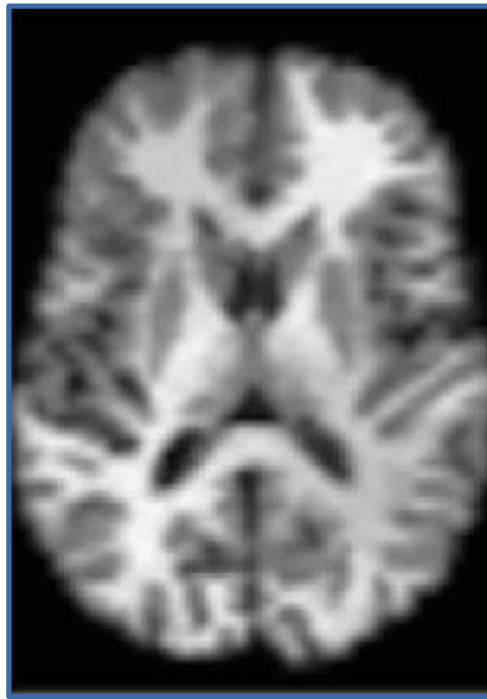
$$\left(\begin{array}{c} \text{Image} \end{array} \right) \mathbf{C} = \left(\begin{array}{ccc} \begin{array}{c} \text{column vector} \end{array} & \dots & \begin{array}{c} \text{column vector} \end{array} \\ \vdots & & \vdots \\ \begin{array}{c} \text{column vector} \end{array} & & \begin{array}{c} \text{column vector} \end{array} \end{array} \right) = \mathbf{L} + \mathbf{S}$$

Low-rank + sparse decomposition example

Input



Low-Rank



Sparse



Now we can work with “almost-normal” images!

Summary

Multiple possibilities to deal with image differences:

The classics: mutual information, normalized cross correlation

Explicit modeling:

- parametric (e.g., logistic curve)
- non-parametric (metamorphosis)
- cost-function masking

Data-driven modeling:

- image analogies through dictionary learning
- creating “normal images” using low-rank + sparse

Which method to use will of course be application-dependent.

Questions?

Questions?