


## Hands on ...

Reconstruction From
Projection


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An Analogy


## Agenda

- Reconstruction from projections (general)
- projection geometry and radon transform
- Reconstruction methodology
- Backprojection, (Fourier slice theorem), Filtered Backprojection.
- Reconstruction examples


## Introduction

- Only photography (reflection) and planar xray (attenuation) measure spatial properties of the imaged object directly.


- Otherwise, measured parameters are some how related to spatial properties of imaged object.
- CT, SPECT and PET (integral projections of parallel rays), MRI (amplitude, frequency and phase) etc...
- Objective: We want to construct the object (image) which creates the measured parameters.


## Problem Statement

- Given a set of 1-D projections and the angles at which these projections were taken.
- How do we reconstruct the 2-D image from which these projections were taken?
- Lets look at the nature of those projections ... ${ }^{\circ}$



## Parallel Beams Projections



## Ray Geometry

- Let $x$ and $y$ be rectilinear coordinates in a given plane.
- A line in this plane at a distance $t_{1}$ from the origin is the given by:

$$
t_{1}=x \cos \theta+y \sin \theta
$$

where $\theta$ is the angle between a unit normal to the line and the x -axis.

## What is Projection ?!!

- Let $g(x, y)$ be a 2-D function.
- A line running through $g(x, y)$ is called a ray.
- The integral of $g(x, y)$ along a ray is called ray integral.
- The set of ray integrals forms a projection defined as :


$$
P_{\theta}\left(t_{1}\right)=\int_{-\infty}^{\infty} \int_{-\infty}^{\infty} g(x, y) \delta\left(x \cos \theta+y \sin \theta-t_{1}\right) d x d y
$$

Impulse sheath placed at the points constituting the ray

## Radon Transform

- Coordinate transformation:
- Radon transform

$$
\begin{aligned}
P_{\theta}(t) & =\int_{-\infty}^{\infty} \int_{-\infty}^{\infty} g(x, y \\
& =\int_{-\infty}^{\infty} g(t, s) d s
\end{aligned}
$$

## Radon Space

- Projections with different angles are stored in sinogram (raw data).
- Each vertical line in a sinogram is a projection with a different angle



## $\theta \in[0, \pi$

## The Myth ©f



Since Radon transform is a group of projections which are basically line integrals, the difference between the projection at $\theta_{\mathrm{o}}$ and $\theta_{\mathrm{o}}+\pi$ will be the direction of the integration.

## The Fourier Slice Theorem

- This theorem relates the 1D Fourier Transform of a projection and the 2D Fourier transform of the object. It relates the Fourier transform of the object along a radial line.

$$
S_{\theta}(f)=\mathfrak{J}_{1 D}\left\{P_{\theta}(t)\right\}=\int_{-\infty}^{\infty} P_{\theta}(t) e^{-j 2 \pi f t} d t
$$



## The Fourier Slice Theorem

- This theorem relates the 1 D Fourier Transform of a projection and the 2 D Fourier transform of the object. It relates the Fourier transform of the object along a radial line.


Space Domain

For the reconstruction to be made it is common to determine the values onto a square grid by linear interpolation from the radial points. But for high frequencies the points are further apart resulting in image
degradation.


Frequency Domain

## The Fourier Slice Theorem

Space Domain
Frequency Domain
$S(f, \theta)$


## A Problem



- All projections contribute to low freqencies


## Solution:


use filtered projection



## Tasks :-

- Scanner simulation
- Phantom Generation
- Projections computation
- Reconstruction from projections
- Analysis:
- Experiment 1: the effect of filter type.
- Experiment 2: the effect of number of projections.
- Experiment 3: the effect of number of rays


## Scanner Simulation - Phantom Generation

- Given the spatial support of our phantom.
- We assume that our phantom is constructed of a set of ellipses, each has the following parameters:
- Intensity, ellipse center $\left(x_{0}, y_{0}\right)$, ellipse major and minor axes length ( $a, b$ ), and the orientation ( $\varphi$ i.e. rotation angle)
function phantom_img = generate_phantom(ellipse_parameters, rows, cols)



## Scanner Simulation - Phantom Generation

```
%% intialization of our phantom
phantom_img = zeros(rows,cols);
* the spatial support (normalized to -1->1
xmid = (cols-1)/2;
ymid = (rows-1)/2;
x_range = ((0:cols-1) - xmid)./xmid;
#_range = ((rows-1:-1:0) - ymid)./Fmid; sthe origin of the image is the left
    *lower corner instead of the upper
    sone
% defining the grid points of our phantom
[x,y] = meshgrid(x_range, Y_range);
% getting the xy coordinates and the phantom flatten in one vector
x = x(:);
Y = F(:);
phantom_img = phantom_img(:);
* defining the grid points of our phantom
\([\mathrm{x}, \mathrm{y}]=\) meshgrid(X_range, \(\overline{\mathrm{Y}}\) _range) ;
\% getting the \(x y\) coordinates and the phantom flatten in one vector
\(\mathrm{x}=\mathrm{x}(\mathrm{l})\);
\(\mathrm{y}=\mathrm{y}(:)\);
phantom_img = phantom_img(:);
* lower corner instead of the upper sone
```




## Scanner Simulation - Phantom Generation

```
8% now lets loop over all ellipses to find the corresponding phantom points
for i = 1 : size(ellipse_parameters,1)
    * the parameters of current ellipse
    A = ellipse_parameters(i,1);
    a = ellipse_parameters(i,2);
    b = ellipse_parameters(i,3);
    x0 = ellipse_parameters(i,4);
    #O = ellipse_parameters(i,5);
    phi = ellipse_parameters(i,6);
    * lets translate the phantom coordinates to be centered at the ellipe's
    * center
    cur_x = x - x0;
    cur_y = y - y0;
    * lets rotate the translated phantom coordinates to align the x-axis
    * with the ellipse's horizontal semi-axis and the y-axis with the
    * ellipse's vertical semi-axis
    rotation_matrix = [ cosd(phi) sind(phi);
        -sind(phi) cosd(phi)];
    pts = [cur_x' ; cur_y'];
    pts = rotation_matrix * pts ;
    cur_x = pts(1,:);
    cur_y = pts(2,:);
% lets see which points in the phantom that will belong to the current 
```


## Scanner Simulation - Phantom Generation

| ellispes_parameters $=$ |  |  |  |  |  |
| ---: | ---: | ---: | ---: | ---: | ---: |
| 1.0000 | 0.6900 | 0.9200 | 0 | 0 | 0 |
| -0.8000 | 0.6624 | 0.8740 | 0 | -0.0184 | 0 |
| -0.2000 | 0.1100 | 0.3100 | 0.2200 | 0 | -18.0000 |
| -0.2000 | 0.1600 | 0.4100 | -0.2200 | 0 | 18.0000 |
| 0.1000 | 0.2100 | 0.2500 | 0 | 0.3500 | 0 |
| 0.1000 | 0.0460 | 0.0460 | 0 | 0.1000 | 0 |
| 0.1000 | 0.0460 | 0.0460 | 0 | -0.1000 | 0 |
| 0.1000 | 0.0460 | 0.0230 | -0.0800 | -0.6050 | 0 |
| 0.1000 | 0.0230 | 0.0230 | 0 | -0.6060 | 0 |
| 0.1000 | 0.0230 | 0.0460 | 0.0600 | -0.6050 | 0 |



## Scanner Simulation - Projections Generation

- To be able to study different reconstruction techniques, we first needed to write a program that take projections of a known image.
- Basically, we take the image (which is just a matrix of intensities), rotate it, and sum up the intensities.
- In MATLAB this is easily accomplished with the 'imrotate' and 'sum' commands.
- But first, we zero pad the image so we don't lose anything when we rotate.

```
8% after padding the image, do the following to generate the projections
thetas = 0:180;
no_of_rays = 300;
projections = zeros(length(thetas), no_of_rays);
for i = 1 : length(thetas)
    rotated_phantom = imrotate(padded_phantom_image, theta(i), 'bilinear','crop');
    projections(:,i) = (sum(rotated_phantom))';
end
```


# Scanner Simulation - Projections Generation from 0 to $\pi$ 



Projections from 0 to 0 degrees



Current Rotated Image


## Scanner Simulation - Projections Generation from 0 to $2 \pi$



Projections from 0 to 0 degrees



Current Rotated Image


## Reconstruction From Projections

- Given the projections, we first filter them as shown below.

```
* number of rays, which corresponds to number of samples in the discretized
* 1D projection
N = size(projections,1);
* sampling the frequency w = 2*pi*f
w= -pi : (2*pi)/N : pi-(2*pi)/N: % -pi to pi
* shifting the response to 0 to 2*pi
filter_response = fftshift(abs(w));
* number of projections
nProjections = size(projections,2);
filtered_projections = zeros(size(projections));
for i = 1:nProjections
    * filter in the frequency domain
    S_f = fft(projections(:,i));
    filtered_S_f = S_f.*filter_response';
    * return to t-theta domain
    filtered_projections(:,i) = ifft(filtered_S_f);
end
* Remove any remaining imaginary parts
filtered_projections = real(filtered_projections);
```


## Reconstruction From Projections

- Given the angles where the projections were taken, and the filtered projections, the following will reconstruct an estimate of the original image.

* find the middle index of the projections center $=($ nProjections +1$) / 2$;
* set up $x$ and $y$ matrices
$\mathrm{x}=1$ :nProjections;
$y=1: n P r o j e c t i o n s ;$
$[\mathrm{X}, \mathrm{Y}]=$ meshgrid( $\mathrm{x}, \mathrm{y})$;
* having the origin in the middle of the grid
xproj $=\mathrm{X}-($ nProjections+1)/2;
yproj $=Y$ - (nProjections+1)/2;
reconstructed_image $=$ zeros(nProjections,nProjections);
for $i=1: n P r o j e c t i o n s$
* figure out which projections to add to which spots
cur_points $=$ round(center + xproj*cos(thetas(i)) + yproj*sin(thetas (i)));
* if we are "in bounds" then add the point
cur_reconstruction $=$ zeros (nProjections, nProjections);
spot $=$ find ((cur_points $>0) \varepsilon$ (cur_points $<=$ N));
new_points = cur_points (spot);
cur_reconstruction(spot) = filtered_projections(new_points(:),i);
*keyboard
reconstructed_image $=$ reconstructed_image + cur_reconstruction;
Point on the current radial line which corresponds to the 1D fourier transform of the current projection
end
reconstructed_image $=$ reconstructed_image./nProjections;


## Experiment One

## Studying the effect of using different filter types compared to the unfiltered case.

## Reconstruction using unfiltered projections




Reconstruction of the projection at 0 degrees



## Reconstruction using Ramp filter




Reconstruction of the projection at 0 degrees



## Reconstruction using LPF filter



## Reconstruction using Butterworth filter



Filtered Projections using Butterworth Filter (Low-Pass Filter)


Reconstruction of the projection at 0 degrees



## Reconstruction using Sinusoidal filter






## Reconstruction using Ramp filter vs unfiltered case




Reconstructed - ramp filter



## Reconstruction using LPF filter vs unfiltered case






Reconstruction using Butterworth filter vs unfiltered

## case

Original image


Reconstructed - unfiltered


Reconstructed - butterworth filter


Butterworth filter frequency response


Reconstruction using Sinusoidal filter vs unfiltered case


Reconstructed - unfiltered


Reconstructed - sinusoidal filter


Sinusoidal filter frequency response


## Experiment Two

## Studying the effect of reconstruction using different number of projections

## Reconstruction using different number of projections

Using sinusoidal filter and number of rays equal to image number columns



Reconstruction using 1 projections


## Quantifying the reconstruction error

Mean square error using different number of projections


## Experiment Three

## Studying the effect of reconstruction using different number of rays

## Reconstruction using different number of rays

Using sinusoidal filter and fixed number of projections


## Quantifying the reconstruction

## error




