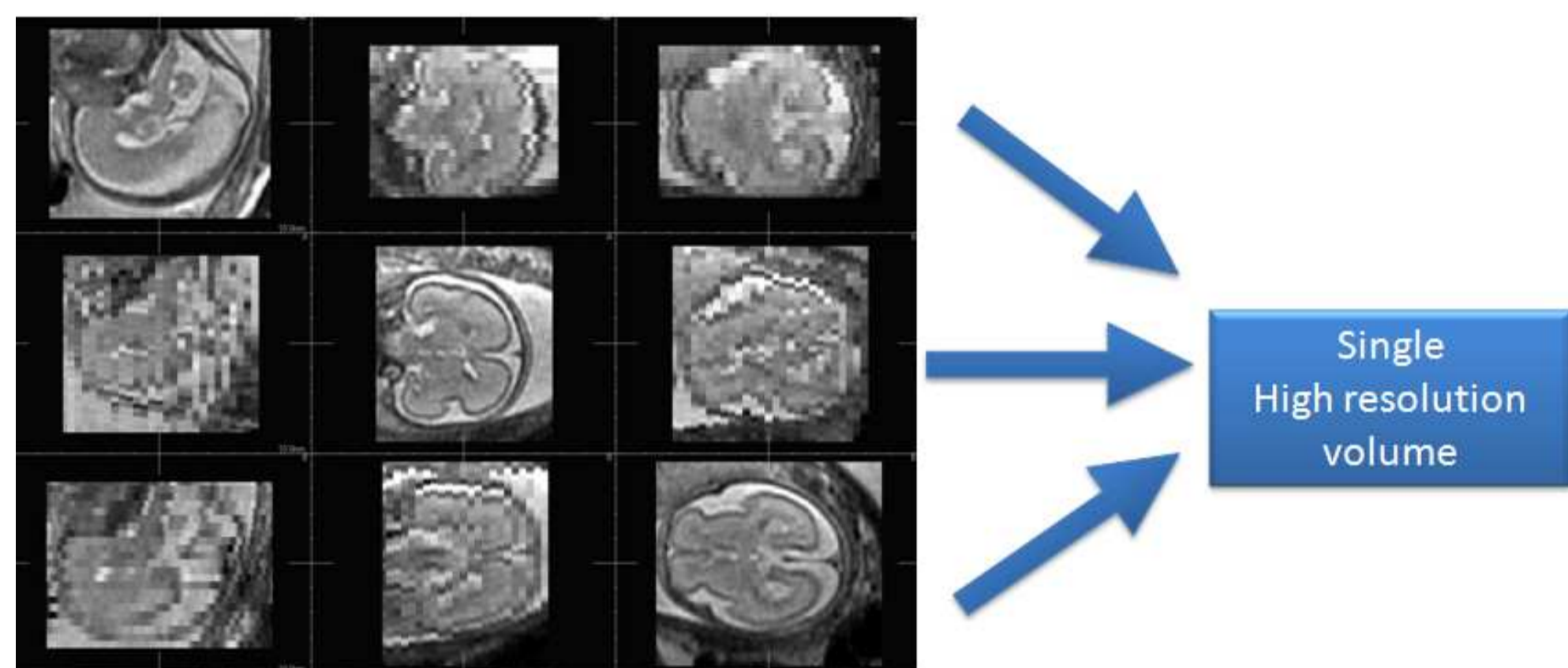


High-Resolution Reconstruction



Imaging moving subjects remains an open issue for Magnetic Resonance Imaging (MRI). Several clinical imaging protocols make use of multiple orthogonal 2D multi-planar acquisitions with non-isotropic voxel size for brain studies. A registration-based method to compound multiple orthogonal sets of 2D fetal MRI slices into a single isotropic high resolution volume have been proposed in [2]. It is composed of the following steps:

- rigid registration of 2D slices,
- relative image contrast correction,
- local approach for image reconstruction.

In this work, we focus on the final image reconstruction step and we propose a new example-based super resolution approach based on the non-local means (NLM) framework [1] in order to improve reconstructed image quality.

Super-Resolution

SR modeling

The most common SR approaches consist in modeling the physical problem and to invert it. These approaches use a generic observation model such as:

$$\mathbf{y}_r = DBW_r\mathbf{x} + \mathbf{n}_r \quad \text{for } 1 \leq r \leq n \quad (1)$$

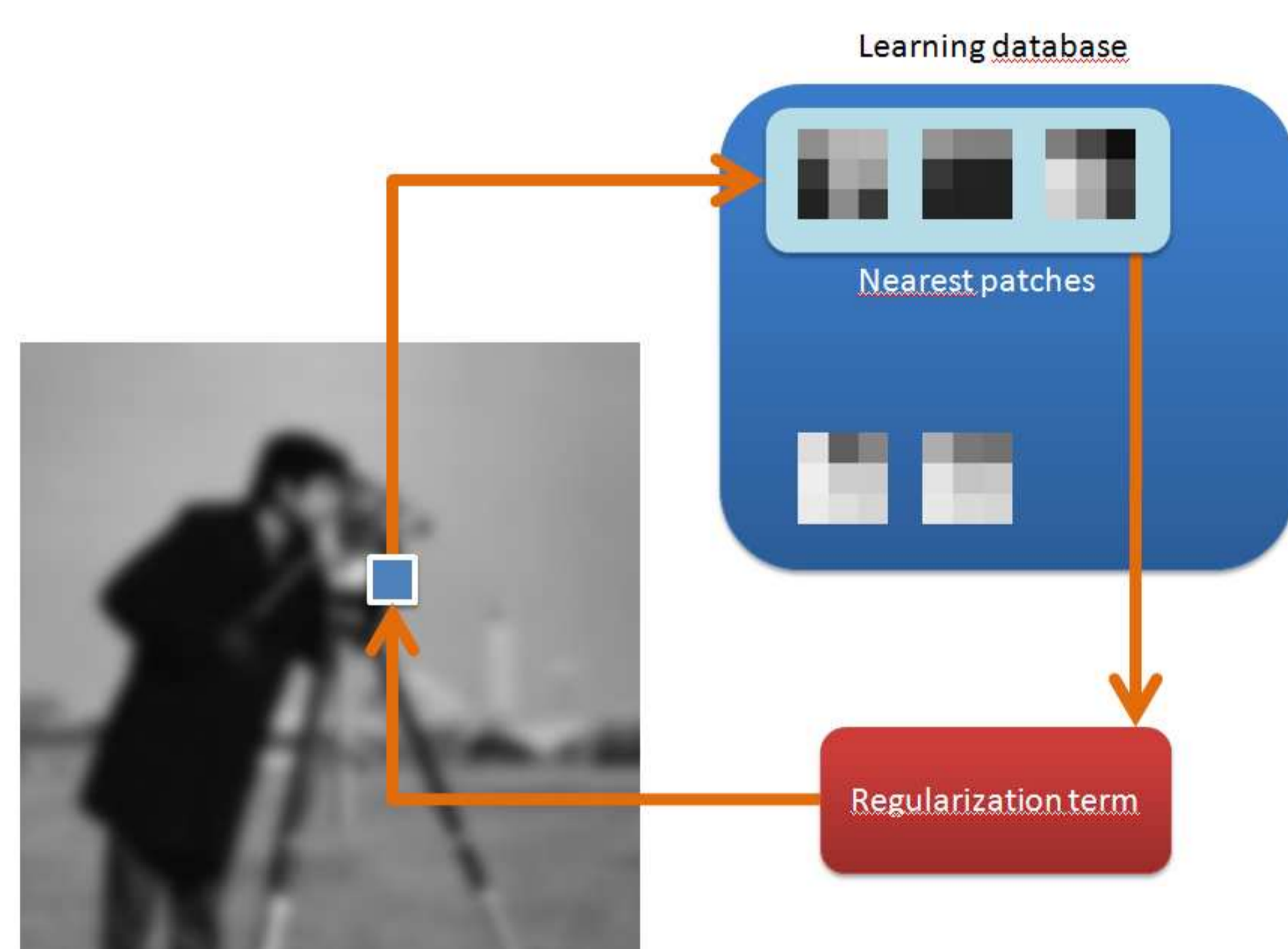
where \mathbf{y}_r , $r \in \{1 \dots n\}$ denotes the low resolution (LR) images, \mathbf{x} is the high resolution (HR) image, \mathbf{n}_r represents observation noise, D is the subsampling matrix, B a blur matrix, W_r is the geometric transformation of r th low resolution image.

The HR image is computed by considering the following equation:

$$\hat{\mathbf{x}} = \arg \min_{\mathbf{x}} \mathcal{L}(\mathbf{x}, \mathbf{y}, H) + \lambda \mathcal{R}(\mathbf{x}). \quad (2)$$

$\mathcal{L}(\mathbf{x}, \mathbf{y}, H) = \sum_r \|\mathbf{y}_r - H_r\mathbf{x}\|^2$ is a data term related to the physical model and $\mathcal{R}(\mathbf{x})$ is a regularization term.

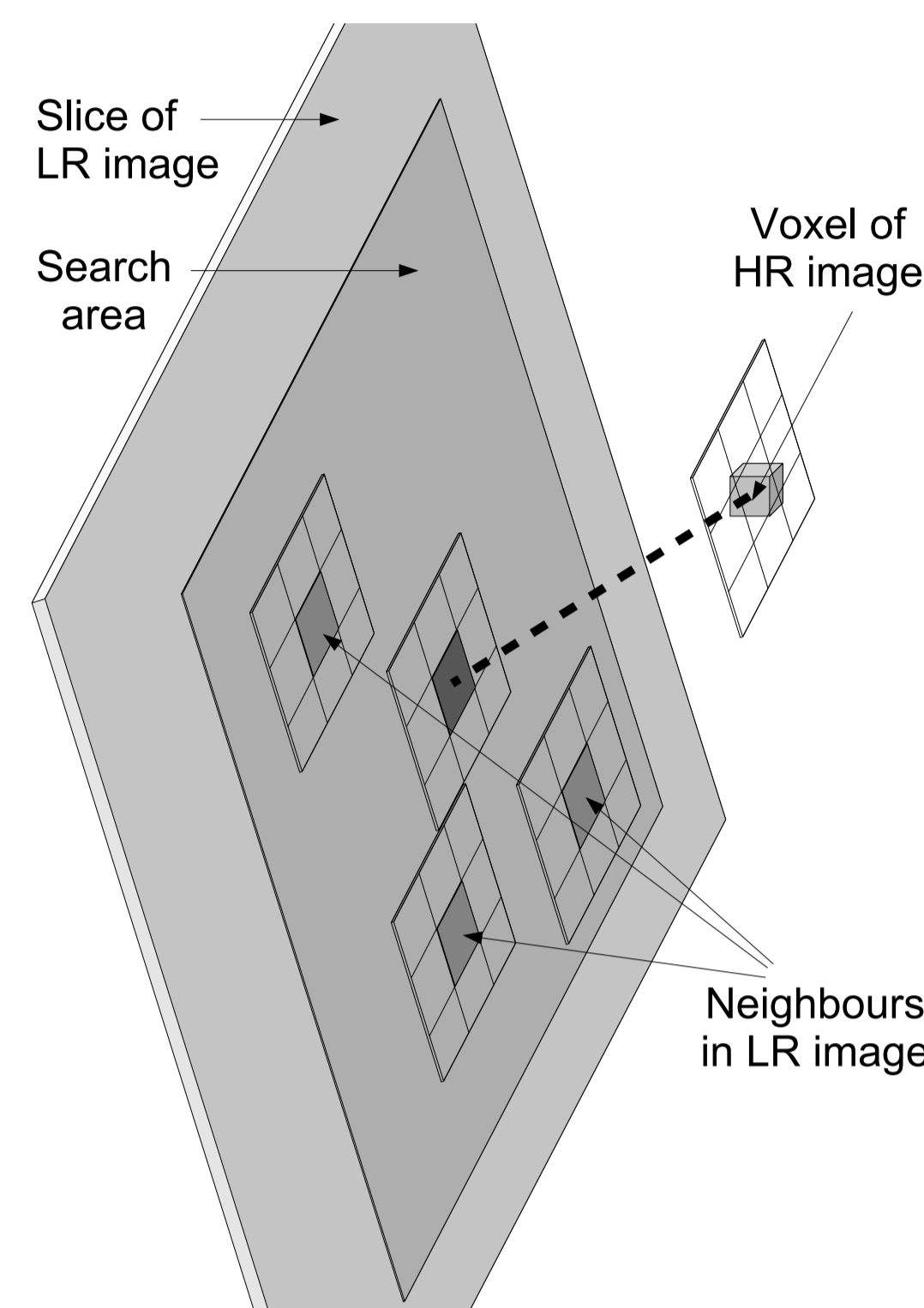
Example-based SR methods



$$\mathcal{R}(\mathbf{x}, \mathcal{E}) = \sum_{\mathbf{v}, k \in \Omega(\mathbf{v})} w_{\mathbf{v}, k} \|f(\mathbf{x}(\mathbf{v})) - \mathcal{E}_{\mathbf{v}, k}\|^2 \quad (3)$$

where $f(\mathbf{x}(\mathbf{v}))$ is an operator on the HR image \mathbf{x} at the voxel \mathbf{v} , $\Omega(\mathbf{v})$ is a neighborhood of \mathbf{v} , \mathcal{E} is the learning database, $\mathcal{E}_{\mathbf{v}, k}$ is a element of \mathcal{E} related to \mathbf{v} and $w_{\mathbf{v}, k}$ is a local weight. It is important to note that in example-based methods the regularization term \mathcal{R} depends on the learning database \mathcal{E} .

Proposed Reconstruction Approach



A new regularization term

- We assume that 2D slices of LR images contain relevant examples of the HR image reconstruction.
- The set of LR images is then considered as a relevant candidate to be the learning database \mathcal{E} .
- The regularization term can be seen as a similarity constraint between the voxels of HR image and closest examples in the LR images:

$$\mathcal{R}(\mathbf{x}, \mathcal{E}) = \sum_{\mathbf{v}} w_{\mathcal{R}}(\mathbf{v}) \|\mathbf{x}(\mathbf{v}) - d_{NLM}(\mathbf{x}(\mathbf{v}), \mathcal{E})\|^2$$

$$d_{NLM}(\mathbf{x}(\mathbf{v})) = \sum_{k \in \Omega(\mathbf{v})} w_{NLM}(\mathbf{v}, k) \mathbf{y}(k)$$

where $\Omega(\mathbf{v})$ corresponds to the neighborhood of the voxel \mathbf{v} in the LR images \mathbf{y} .

FIGURE 1: Link between example patterns in LR images and voxel in HR image.

Results

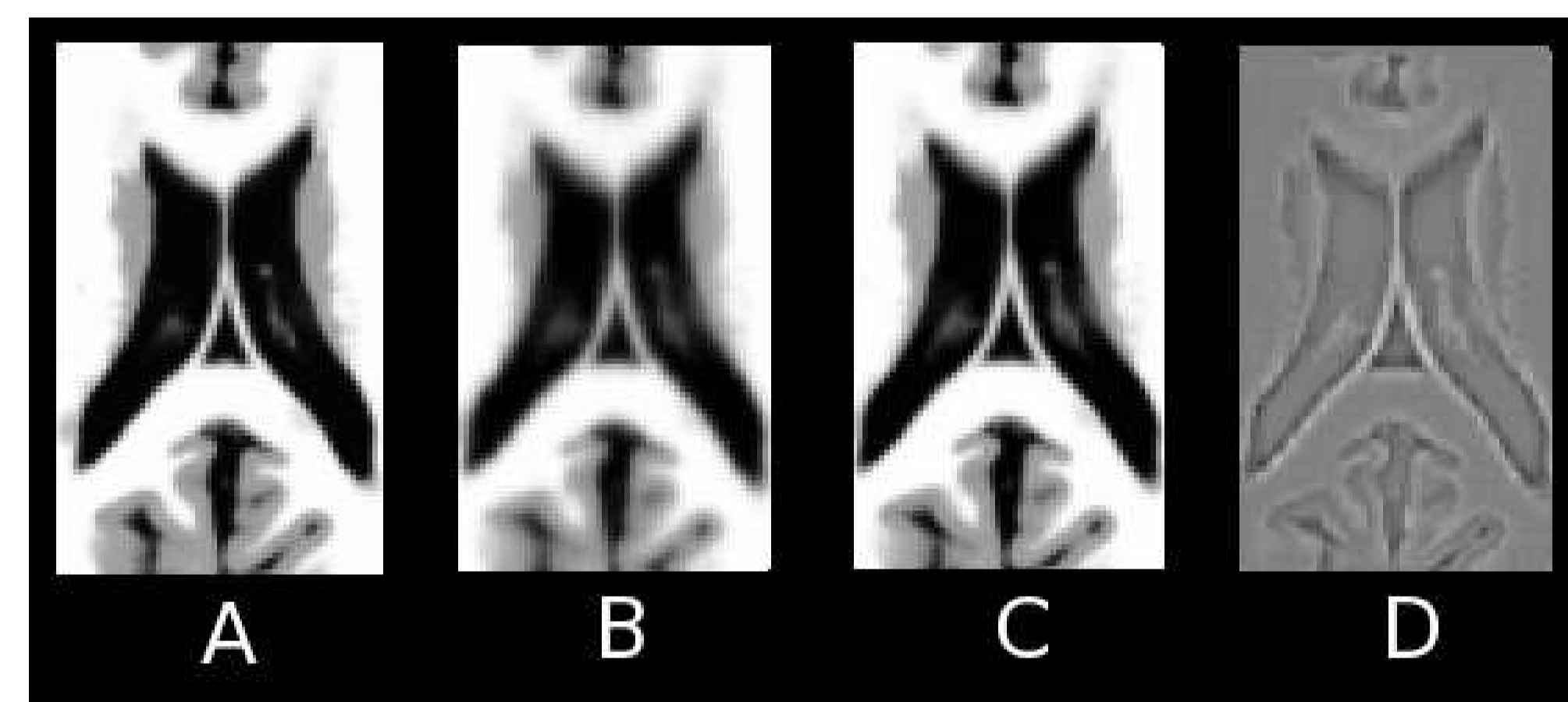


FIGURE 2: Details of reconstructed images (simulation on Brainweb images). From left to right: A) ground truth, B) reconstructed image using local interpolation [2], C) proposed approach, D) difference between C and B.

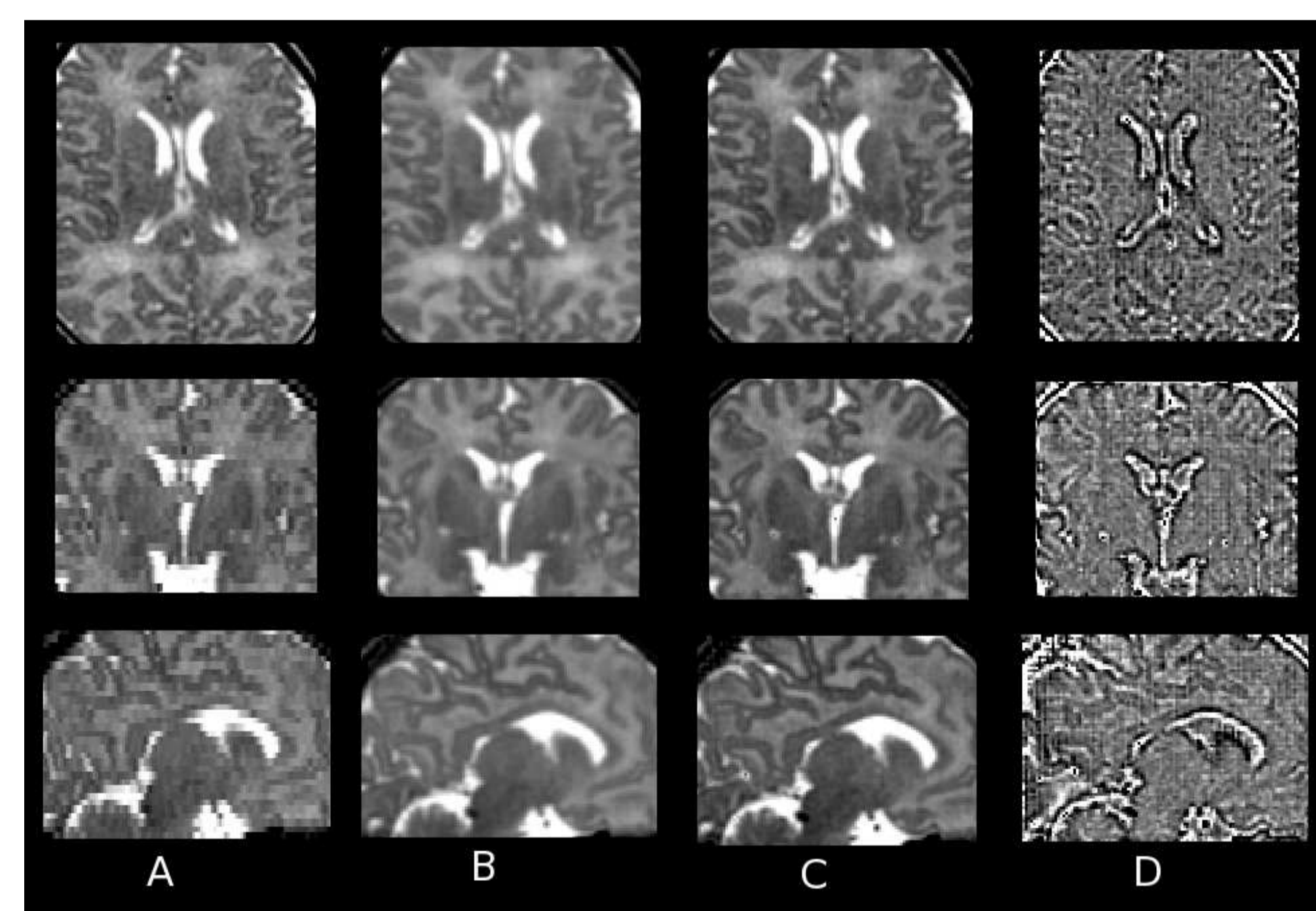


FIGURE 3: Details of reconstructed infant MR images. From left to right: A) original low resolution image, B) reconstructed image using local interpolation [2], C) proposed approach, D) difference between C and B.

References

- [1] Buades, A. and Coll, B. and Morel, J.M. A review of image denoising algorithms, with a new one *Multiscale Modeling & Simulation*, 4(2):490–530, 2005.
- [2] Rousseau, F. *et al.* Registration-Based Approach for Reconstruction of High-Resolution in Utero Fetal MR Brain images *Academic Radiology*, 13(9):1072–1081, 2006.

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